Two-photon fluorescence imaging of intracellular hydrogen peroxide with chemoselective fluorescent probes

The Harvard community has made this article openly available. Please share how this access benefits you. Your story matters

Citation


Published Version
doi:10.1117/1.JBO.18.10.106002

Citable link
http://nrs.harvard.edu/urn-3:HUL.InstRepos:13347494

Terms of Use
This article was downloaded from Harvard University’s DASH repository, and is made available under the terms and conditions applicable to Other Posted Material, as set forth at http://nrs.harvard.edu/urn-3:HUL.InstRepos:dash.current.terms-of-use#LAA
Two-photon fluorescence imaging of intracellular hydrogen peroxide with chemoselective fluorescent probes

Hengchang Guo
Hossein Aleyasin
Scott S. Howard
Bryan C. Dickinson
Vivian S. Lin
Renee E. Haskew-Layton
Chris Xu
Yu Chen
Rajiv R. Ratan
Two-photon fluorescence imaging of intracellular hydrogen peroxide with chemoselective fluorescent probes

Hengchang Guo,a,b Hossein Aleyasin,b Scott S. Howard,c,d Bryan C. Dickinson,e Vivian S. Lin,f Renee E. Haskew-Layton,1 Chris Xu,c Yu Chen,a and Rajiv R. Ratanb

Department of Chemistry and Chemical Biology, Harvard University, Department of Chemistry and Chemical Biology, Cambridge, Massachusetts 02138

School of Applied and Engineering Physics, Ithaca, New York 14853

Fischell Department of Bioengineering, College Park, Maryland 20742

Department of Electrical Engineering, Notre Dame, Indiana 46556

Burke Medical Research Institute, 785 Mamaroneck Avenue, White Plains, New York 10605

Address all correspondence to: Chris Xu, Cornell University, School of Applied and Engineering Physics, 276 Clark Hall, Ithaca, New York 14853. Tel: +1-607-255-1460; E-mail: chris.xu@cornell.edu; or Yu Chen, University of Maryland, Fischell Department of Bioengineering, College Park, Maryland 20742. Tel: +1-301-405-3439; Fax: +1-240-554-1688; E-mail: yuchen@umd.edu; or Rajiv R. Ratan, Burke Medical Research Institute, 785 Mamaroneck Avenue, White Plains, New York 10605. Tel: +1-914-597-2851; Fax: +1-914-597-2225; E-mail: rrr2001@med.cornell.edu

Abstract. We present the application of two-photon fluorescence (TPF) imaging to monitor intracellular hydrogen peroxide (H2O2) production in brain cells. For selective imaging of H2O2 over other reactive oxygen species, we employed small-molecule fluorescent probes that utilize a chemoselective boronate deprotection mechanism. Peroxyfluor-6 acetoxymethyl ester detects global cellular H2O2 and mitochondria peroxy yellow 1 detects mitochondrial H2O2. Two-photon absorption cross sections for these H2O2 probes are measured with a mode-locked Ti:sapphire laser in the wavelength range of 720 to 1040 nm. TPF imaging is demonstrated in the HT22 cell line to monitor both cytoplasmic H2O2 and localized H2O2 production in mitochondria. Endogenous cytoplasmic H2O2 production is detected with TPF imaging in rat astrocytes modified with d-amino acid oxidase. The TPF H2O2 imaging demonstrated that these chemoselective probes are powerful tools for the detection of intracellular H2O2. © The Authors. Published by SPIE under a Creative Commons Attribution 3.0 Unported License. Distribution or reproduction of this work in whole or in part requires full attribution of the original publication, including its DOI. [DOI: 10.1117/1.JBO.18.10.106002]

Keywords: two-photon fluorescence imaging; hydrogen peroxide; reactive oxygen species; fluorescent probe; oxidative stress; molecular imaging.

Paper 130259R received Apr. 17, 2013; revised manuscript received Aug. 16, 2013; accepted for publication Aug. 28, 2013; published online Oct. 1, 2013.

1 Introduction

Hydrogen peroxide (H2O2), a common reactive oxygen species (ROS) found in biological systems, is now recognized as an intracellular second messenger for cellular signaling that exerts diverse physiological and pathological effects.1,2,13 The aberrant production or accumulation of H2O2 within cellular mitochondria over time due to oxidative stress or genetic mutation is connected to serious pathological conditions including cancer,3 diabetes,9 and neurodegenerative diseases such as Alzheimer’s, Parkinson’s, and Huntington’s diseases, as well as stroke.10-12 In addition, H2O2 is involved in therapeutic processes such as wound healing, stem cell proliferation, and an adaptive response in astrocytes leading to neuronal protection.12,15,16

A substantial challenge in elucidating the diverse roles of H2O2 in complex biological environments is the lack of methods to determine the spatial and temporal dynamics of this reactive oxygen metabolite in living systems. For the detection of ROS production in vitro, several fluorescent probes have been developed based on small molecules, fluorescent proteins, and nanoparticles.3,14-19 Among these technologies, small molecule probes offer an attractive approach to ROS detection due to their general compatibility with an array of biological systems without external activating enzymes and genetic manipulation. However, traditional small molecule probes such as dichloro-fluorescein (DCF) derivatives detect multiple types of reactive small molecules, including other ROS such as superoxide radical (O2·−), hydroperoxy radical (HO2·), singlet oxygen (1O2), peroxy radical (RO2·), and reactive nitrogen species;16 they are not specific for H2O2. In addition, DCF derivatives cannot be targeted to specific intracellular compartments.15 To overcome the disadvantages of existing methods for detecting ROS, new chemoselective fluorescent indicators featuring a boronate-based molecular detection mechanism have been developed,3 which provide improved selectivity for H2O2 over related ROS, particularly superoxide, nitric oxide, and hydroxyl radical. These probes include peroxyfluor-2 (PF2), peroxy yellow 1 (PY1), peroxy orange 1 (PO1), peroxyfluor-6 acetoxymethyl ester (PF6-AM), mitochondria peroxy yellow 1 (MitoPY1), etc.3,14,20-23

However, conventional confocal microscopy has limitations for use in real time in vivo H2O2 imaging, including photodamage, photobleaching, and limited imaging depth. Furthermore, prolonged visible light exposure can result in artifactual ROS generation and signal amplification.23 Therefore, two-photon imaging of H2O2 offers an attractive alternative to overcome many of these limitations.26-27 We report two-photon fluorescence (TPF) imaging for the detection of intracellular cytoplasmic
and mitochondrial H$_2$O$_2$ production in live cells using a variety of next-generation boronate-based probes such as PF6-AM and MitoPY1. Two-photon absorption (TPA) cross sections of these probes were measured with a Ti:sapphire laser by comparison with the TPA cross section of fluorescein.\textsuperscript{26,28} To our knowledge, this is the first two-photon characterization of these particular chemoselective probes and provides a clear example for the detection of intracellular H$_2$O$_2$ production with TPF imaging.

2 Materials and Methods

2.1 Chemoselective Fluorescent Probes

We characterized a series of previously reported chemoselective probes with three useful colors: green (PF2 and PF6-AM), yellow (PY1 and MitoPY1), and orange (PO1). Figure 1 illustrates reaction of H$_2$O$_2$ with these probes, which are based on fluorescein/rhodamine derivatives. The aryl boronate to phenol chemical switch is utilized for selective detection of H$_2$O$_2$ over other ROS. Upon reaction with H$_2$O$_2$, a highly fluorescent product is released and can be assayed by fluorescence imaging. To improve the cell membrane permeability and trap the probe in the cytosol, PF6-AM was modified from PF6 with acetoxy-methyl ester groups.\textsuperscript{2,26} Upon penetration of the cell membrane, PF6-AM is deprotected by intracellular esterases, releasing the dianionic PF6 that is then trapped in the cytosol [Fig. 1(e)]. MitoPY1 [Fig. 1(d)] was derived from PY1 to include a combination of a boronate-based switch and a mitochondrial-targeting phosphonium moiety for the detection of H$_2$O$_2$ localized to cellular mitochondria.\textsuperscript{18}

2.2 TPA Measurement

A basic parameter to characterize a fluorophore for TPF imaging is the TPA cross section. TPA spectra were measured using a Ti:sapphire laser (Spectra Physics Mai Tai HP) operating at 720 to 1040 nm, 100 fs pulse width, and 80 MHz repetition rate. The scheme of experimental setup was described in Xu and Webb.\textsuperscript{28} Before the measurement, we verified that the TPF intensity increases with the square of the excitation power.

TPF intensity is related to spatial dependence and temporal dependence such as laser parameters and system collection condition.\textsuperscript{28} A direct measurement of TPA cross section is difficult. Therefore, absolute TPA cross section values of fluorescent probes ($\delta_P$) were calculated by comparison with the TPF intensity of fluorescein ($\delta_F$) in Eq. (1):\textsuperscript{28}

$$\delta_P = \frac{\delta_F F_P \Phi_P c_P \Phi_{P-PMT}}{F_F \Phi_F c_F \Phi_{F-PMT}},$$

where $F_P$ and $F_F$ are the fluorescence intensity measured with a photon counting photomultiplier tube (PMT) at the same laser power excitation, $\Phi_P$ and $\Phi_F$ are the two-photon-excited fluorescence quantum yields of the probes assumed to be same to that of single-photon excited, $c_P$ and $c_F$ are the concentrations of the probes, $\Phi_{P-PMT}$ and $\Phi_{F-PMT}$ are the quantum efficiency of the PMT (Hamamatsu R7600U-200) obtained from the manufacturer’s data. The system collection efficiency, estimated to be the same for the probes, are based on its fluorescence emission spectrum, the measured numerical aperture (NA) and transmission of the objective lens, and the transmission of the filters.\textsuperscript{28} The fluorescent probes were measured with the same measurement conditions as fluorescein, therefore these probes were measured with the same measurement conditions as fluorescein, therefore these
measurements can be used to calculate TPA cross section without explicitly characterizing pulse shape by comparing measured values to those found in Ref. 28.

PF2, PY1, PO1, MitoPY1, and DCF were diluted to form a 20 μM solution in 1x phosphate buffered saline (PBS) buffer. We then added high concentrations of H$_2$O$_2$ (100 μM) to ensure complete deprotection. PF6-AM (20 μM) in 1x PBS buffer was incubated with both H$_2$O$_2$ (100 μM) and esterase (10 U/mL) from rabbit liver (Sigma–Aldrich #040566) to deprotect the boronate and the AM-esters.

2.3 Confocal and Two-photon Microscopy

H$_2$O$_2$ imaging was performed with a commercial laser scanning inverted microscope system (Zeiss 710NLO) including configuration both for confocal and TPF microscopy. This system was equipped with a 488-nm argon laser and a Ti:sapphire laser (Coherent Chameleon Vision II) with 690- to 1080-nm wavelength, 140-fs pulse width, and 80-MHz repetition rate. We operated the Ti:sapphire laser at 770 nm, a wavelength for TPF imaging of PF6-AM, MitoPY1, and Hoechst 33342. A 20 × 0.80 NA objective (Zeiss Plan-Apochromat) was employed to focus the excitation laser beam onto cells and was also used for fluorescence collection into the PMTs. A prism-based 34-channel QUASAR detection unit was used for tunable spectral band-width collection without traditional band-pass filters. A 5% CO$_2$ circulation and 37°C thermal chamber was used for live cell imaging.

2.4 Cell Culture

All animal procedures were performed according to protocols approved by the Institutional Animal Care and Use Committee of the Weill Medical College of Cornell University. The HT22 cell, an immortal neuroblast line originated from hippocampal neurons, and primary rat astrocytes were cultured in 35-mm Petri dishes with a cover-glass at the bottom.

Primary astrocyte cultures were prepared from the cerebral cortices of Sprague-Dawley rat pups (P1-3) as described in Haskew-Layton et al. 1 In brief, astrocyte cultures were grown for about 2 weeks until reaching confluence in minimal essential medium (Invitrogen) supplemented with 10% horse serum and 25 U/mL penicillin plus 25 μg/mL streptomycin. Once confluent, the astrocytes were treated with 8 μM cytosine-β-arabino-furanoside (Ara-C), a mitotic inhibitor for primary astrocyte cultures. This result demonstrates that PF6-AM is capable of detecting cytoplasmic H$_2$O$_2$. Figures 3(c) and 3(d) demonstrate the concentration of d-alanine added. Following DAAO-transduction, astrocytes were incubated with 5 μM PF6-AM and Hoechst 33342. d-Alanine (2 mM) stimulated H$_2$O$_2$ production in DAAO astrocytes was then detected; the cells were supplemented with the DAAO cofactor FAD (2.5 μM).

3 Results and Discussions

3.1 TPA Spectrum

The two-photon activation times, single-photon absorption and emission peaks, and quantum yields of the probes were measured and are shown in Table 1. Activation time refers to the average time when the TPF intensity increases to 1/e of the saturation intensity. This activation time is related to the deprotection efficiency. Compared with the commonly used nonspecific probe DCF, the chemoselective probes demonstrated much faster responses to H$_2$O$_2$.

Figure 2 shows single-photon absorption and fluorescence emission spectra, and absolute values of TPA cross sections for the H$_2$O$_2$ probes PF2, PY1, PO1, MitoPY1, and PF6-AM. As a comparison, Fig. 2(f) shows the TPA cross section of DCF. The peak cross section values of chemoselective probes are comparable to that of fluorescein, which is sufficiently large for two-photon imaging in vitro or in vivo. To ensure that H$_2$O$_2$ has deprotected the boronate, the TPF spectra were measured at least 1 h after H$_2$O$_2$ addition. Then, the TPA cross section was calculated based on the above Eq. (1) and the parameter in Table 1.

We measured several color probes here so that multicolor imaging can be performed with minimum fluorescence bleed-through with other co-staining dyes. Figure 2 helps us to select co-staining dyes for single excitation wavelength two-photon multicolor imaging.

3.2 TPF Imaging of Intracellular H$_2$O$_2$

Figure 3 shows intracellular TPF imaging of H$_2$O$_2$ in HT22 cells stained with PF6-AM. The cells were incubated in PF6-AM solution for 20 min and the nuclei were stained with Hoechst 33342. Figures 3(a) and 3(b) show the H$_2$O$_2$ concentration increasing in cells after the addition of exogenous H$_2$O$_2$. This result demonstrates that PF6-AM is capable of detecting cytoplasmic H$_2$O$_2$. Figures 3(c) and 3(d) demonstrate

### Table 1: Optical parameters of H$_2$O$_2$ probes

<table>
<thead>
<tr>
<th>Probes</th>
<th>Absorption peak (nm)</th>
<th>Emission peak (nm)</th>
<th>Quantum yields</th>
<th>Activation time$^a$ [min]</th>
</tr>
</thead>
<tbody>
<tr>
<td>PF2</td>
<td>455</td>
<td>515</td>
<td>0.27</td>
<td>3 ± 1</td>
</tr>
<tr>
<td>PY1</td>
<td>520</td>
<td>550</td>
<td>0.12</td>
<td>3 ± 3</td>
</tr>
<tr>
<td>PO1</td>
<td>540</td>
<td>570</td>
<td>0.46</td>
<td>3 ± 3</td>
</tr>
<tr>
<td>MitoPY1</td>
<td>510</td>
<td>530</td>
<td>0.405</td>
<td>24 ± 5</td>
</tr>
<tr>
<td>PF6-AM</td>
<td>460</td>
<td>520</td>
<td>0.94</td>
<td>14 ± 1</td>
</tr>
<tr>
<td>DCF</td>
<td>500</td>
<td>525</td>
<td>0.9 to 0.95</td>
<td>48 ± 1</td>
</tr>
</tbody>
</table>

$^a$ Activation time $\tau$ is obtained from the simulation of this equation sat $− (sat − int) \times \exp (−sx/r)$ using Qtiplot software.
endogenous H$_2$O$_2$ production induced by rotenone, which resulted in bright punctate staining patterns that are likely the sources of H$_2$O$_2$ production.

To improve the signal-to-background ratio and target mitochondrial H$_2$O$_2$ production, we used MitoPY1 for mitochondrial labeling and detection of localized H$_2$O$_2$ production. Figure 4 shows an overlay of TPF imaging of MitoPY1 labeled mitochondrial H$_2$O$_2$ production and MitoTracker Red labeled mitochondria. Rotenone was added to the HT22 cells after they were incubated with 5 μM MitoPY1 for 25 min. Then, MitoTracker Red was added after another 60 min to ensure that MitoPY1 was targeted to the mitochondria in HT22 cells.

Figure 5 shows TPF imaging of cytoplasmic H$_2$O$_2$ production induced by DAAO in astrocytes. PF6-AM and Hoechst 33342 were co-excited with 770-nm laser pulses. The TPA cross section of FAD at 770 nm is only $\times 10^{-3}$ that of PF6AM. Therefore, the fluorescence of FAD is only a weak background signal. The fluorescence intensity in Fig. 5 shows cytoplasmic H$_2$O$_2$ increasing from the time (a) 1 min, (b) 6 min, and (c) 25 min after the addition of D-alanine and FAD.

### 3.3 Discussion

The involvement of H$_2$O$_2$ in cellular signaling related to cancer and neurodegenerative diseases has motivated the development of imaging technologies for measuring intracellular H$_2$O$_2$ concentration and dynamics in cellular compartments. Previous studies have relied on a horseradish peroxidase/Amplex Red substrate system to measure extracellular H$_2$O$_2$ production using a spectrophotometer (Spectramax Plus 384; Molecular Devices). However, DAAO derived H$_2$O$_2$ production provides a controllable scale ideal for intracellular H$_2$O$_2$ measurements. TPF signal intensity is linearly related to the fluorophore concentration. Therefore, TPF imaging provides the possibility for quantification of localized intracellular H$_2$O$_2$ production.
The real-time visualization of $\text{H}_2\text{O}_2$ production is another challenging issue that required a fast response of the fluorescent probes. Here, the chemoselective $\text{H}_2\text{O}_2$ probes showed much faster activation time compared with commercial probes such as DCF. It provides a more accurate technique for flow cytometric analysis of isolated cells or mitochondria and allows for the detection of changes such as cell activation, oxidative status, and cell death. Some probes have been successfully used to study ROS in a variety of biological systems with confocal microscopy. Therefore, the combination of new fluorescent probes for $\text{H}_2\text{O}_2$ and the deep tissue imaging capability of two-photon microscopy may allow direct visualization of $\text{in vivo}$ $\text{H}_2\text{O}_2$ dynamics in cells in their natural environment as well as their response to systematic manipulations.

4 Conclusions
This study introduces chemoselective probes for TPF imaging intracellular $\text{H}_2\text{O}_2$ production. TPA spectra were measured and TPF imaging was successfully demonstrated for cytoplasmic...
and mitochondrial H$_2$O$_2$ production in brain cells using PF6-AM and MitoPY1 probes. The probes showed high sensitivity and fast response to H$_2$O$_2$ detection. With the advantages of chemoselective probes, TPF imaging provides a novel opportunity for real-time monitoring of H$_2$O$_2$ detection and oxidative stress evaluation in live cells and in vivo.

**Acknowledgments**

This work is supported by the National Institutes of Health (NIH) Grant Nos. 2P01AG014930, 3R01 CA133148, R21AG042700, R21DK088066, R21EB012215, Dr. Miriam and Sheldon G. Adelson Medical Research Foundation. B.C.D. is a Fellow of the Jane Coffin Childs Memorial Fund for Medical Research. We acknowledge Christopher J. Chang, Demirhan Kobat, David Rivera, Anthony Found, Li Barie, Jian Zhong, and Jimmy B. Payappilly for technical support and helpful comments.

**References**


