Dissociated multimodal hubs and seizures in temporal lobe epilepsy

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Dissociated multimodal hubs and seizures in temporal lobe epilepsy

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Abstract

Objective: Brain connectivity at rest is altered in temporal lobe epilepsy (TLE), particularly in “hub” areas such as the posterior default mode network (DMN). Although both functional and anatomical connectivity are disturbed in TLE, the relationships between measures as well as to seizure frequency remain unclear. We aim to clarify these associations using connectivity measures specifically sensitive to hubs.

Methods: Connectivity between 1000 cortical surface parcels was determined in 49 TLE patients and 23 controls with diffusion and resting-state functional magnetic resonance imaging. Two types of hub connectivity were investigated across multiple brain modules (the DMN, motor system, etcetera): (1) within-module connectivity (a measure of local importance that assesses a parcel’s communication level within its own subnetwork) and (2) between-module connectivity (a measure that assesses connections across multiple modules).

Results: In TLE patients, there was lower overall functional integrity of the DMN as well as an increase in posterior hub connections with other modules. Anatomical between-module connectivity was globally decreased. Higher DMN disintegration (DD) coincided with higher anatomical between-module connectivity, whereas both were associated with increased seizure frequency. DD related to seizure frequency through mediating effects of anatomical connectivity, but seizure frequency also correlated with anatomical connectivity through DD, indicating a complex interaction between multimodal networks and symptoms.

Interpretation: We provide evidence for dissociated anatomical and functional hub connectivity in TLE. Moreover, shifts in functional hub connections from within to outside the DMN, an overall loss of integrative anatomical communication, and the interaction between the two increase seizure frequency.

Introduction

Temporal lobe epilepsy (TLE) has classically been seen as a disease limited to temporal structures. However, the rise of “connectomics” has changed this view. Connectomics are based on communication between brain areas, which may be measured with multiple imaging modalities. Resting-state functional magnetic resonance imaging (rsfMRI) allows for assessment of correlations between baseline oxygenation patterns, with particular brain areas showing similar fluctuations of activity at rest. One such subnetwork is the default mode network (DMN), consisting of the posterior cingulate cortex (PCC), precuneus, medial frontal cortex, parts of the temporal cortex, and inferior parietal areas. DMN areas have high information throughput and are seen as major functional connectomic “hubs”. If we equate functional connectomics to cars moving between cities, then the underlying highways are their anatomical counterparts. Anatomical connectomics can, among others, be measured by reconstructing white
matter pathways with diffusion MRI and counting the number of fibers connecting different brain areas.

TLE is characterized by altered functional and anatomical connectomics throughout the brain, leading to the current view of TLE as a network disease. The disconnection occurs mainly within the DMN. Anatomical connectivity is decreased globally, but locally increases in DMN regions. In healthy brains, anatomical and functional connectomics largely overlap, particularly in hub regions of the brain. Diseases such as idiopathic epilepsy alter this usually tight-knit relationship. In TLE, disturbed functional connectivity is related to altered white matter integrity, particularly in the posterior DMN. Diseases such as idiopathic epilepsy alter this usually tight-knit relationship. In TLE, disturbed functional connectivity is related to altered white matter integrity, particularly in the posterior DMN. Diseases such as idiopathic epilepsy alter this usually tight-knit relationship. In TLE, disturbed functional connectivity is related to altered white matter integrity, particularly in the posterior DMN. Diseases such as idiopathic epilepsy alter this usually tight-knit relationship.

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In this light, two interesting measures of hubness can be determined using “modularity.” Modularity refers to the extent to which the brain can be divided into maximally intracorrelated subnetworks or modules based on its connectome. This graph theoretical technique yields results similar to independent component analysis (ICA) in rsfMRI. Generally, around four to ten brain modules are found, corresponding to known subsystems (e.g., DMN, motor system). Modular decomposition then allows for extensive investigation of connectivity within and across modules: within-module connectivity refers to an area’s communication within its subnetwork, assessing local importance. Between-module connections link multiple modules, transferring information over the entire network (“connector hubness”). Connector hubness in particular may be implicated in TLE, given that it relates to number of seizures and epilepsy-related protein expression in glioma patients.

We investigate the multimodal connectome in a large cohort of TLE patients. Although we investigate the entire brain, we expect that the DMN is the most affected functional module in TLE. Second, we hypothesize that particularly between-module connectomics relate to patients’ seizure symptoms. Finally, dysfunctional anatomical connectomics are expected to mediate the association between altered functional connectomics and seizure symptoms.

Methods

Participants

Data were analyzed retrospectively after patient visits to Massachusetts General Hospital (MGH) between December 2009 and April 2013. All patients suffered from refractory TLE and were referred for presurgical imaging work-up. Inclusion criteria were age over 18 years and suspected TLE as determined by a specialized team of experienced epileptologists (N. T., A. J. C., C. R., S. M. S.) based on ictal video-EEG in accordance with the epilepsy classification by the International League Against Epilepsy (ILAE). Exclusion criteria were previous surgical intervention and neurological or psychiatric comorbidity. In addition to high-resolution imaging, clinical information was collected by medical chart review. Seizure frequency per month was extrapolated from patients’ medical charts, and was only included when reported within 3 months of scanning date. Twenty-three healthy participants were also included, exclusion criteria being psychiatric or neurological disease and use of medication influencing the central nervous system. Hippocampal volumes were determined using FreeSurfer (http://surfer.nmr.mgh.harvard.edu) automatic segmentation procedures.

Both the retrospective analysis of patient data and prospective inclusion of healthy controls was approved by MGH’s institutional review board, and was performed in accordance with the Declaration of Helsinki. All healthy participants gave written informed consent before participation.

MRI data acquisition

The analysis pipeline is depicted in Figure 1. MRI data were collected using a 3T Siemens (Erlangen, Germany)
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A. rs-fMRI preprocessing

B. MPRAGE registration

C. DTI preprocessing

D. common 1000 parcel surface parcellation

E. adjacency matrix per subject

F. group averaged benchmark modules for both modalities

- average matrix for controls
- average matrix for patients
- control fMRI benchmarks
- patient fMRI benchmarks
- control DTI benchmarks
- patient DTI benchmarks

G. individual modularity & parcel analysis

- high within-module connectivity
- high between-module connectivity

scanner with a 32-channel head coil. Anatomical images (multi-echo magnetization-prepared rapid acquisition with gradient echo [MEMPRAGE]), rsfMRI, and diffusion-weighted images (DTI) were collected. Scanning parameters of the MEMPRAGEs were as follows for patients: repetition time = 2530 msec, echo time = 1.74 msec, flip angle = 7°, field of view = 256, voxel size = 1 × 1 × 1 mm³, 176 volumes; and for controls: repetition time = 2000 msec, echo time = 3.37 msec, flip angle = 10°, field of view = 256, voxel size = 1 × 1 × 1 mm³, 160 volumes. In patients, rsfMRI was collected as follows: repetition time = 3000 msec, echo time = 30 msec, flip angle = 85°, field of view = 72, voxel size = 3 × 3 × 3 mm³, 160 volumes, 8 min acquisition; and controls: repetition time = 3000 msec, echo time = 50 msec, flip angle = 90°, field of view = 128, voxel size = 2 × 2 × 2 mm³, 76 volumes, 6.3 min acquisition, 2 runs. For DTI, scanning parameters for all participants were as follows: repetition time = 3000 msec, echo time = 1000 msec, flip angle = 90°, field of view = 128, voxel size = 1.85 × 1.85 × 1.85 mm, 10 b₀ volumes and 60 directional gradients at b = 700 sec/mm².

rsfMRI analysis

The Lausanne 2008 parcellation scheme was used for analysis of 1000 cortical surface parcels. This parcellation is based on the Desikan atlas, after which the cortical surface is further divided into areas with approximately the same size (1.5 mm³).

During rsfMRI, participants fixated their gaze and were instructed to stay awake without thinking about anything in particular. Participants with more than 3 mm absolute head movement during rsfMRI were excluded. Standard preprocessing of rsfMRI data included (1) discarding the first four volumes of each run to ascertain T1-equilibrium, (2) slice timing correction, (3) head motion correction with FSL, (4) removal of constant offset and linear trend per run, (5) low-pass filtering below 0.08 Hz, (6) regressing out of six motion parameters, average signal of the whole brain, ventricles, and white matter. Participants’ individual functional images were projected onto a template cortical surface, after which a 6 mm full-width half-maximum (FWHM) smoothing kernel was applied to the surface data, and data were down sampled to 4 mm resolution. Average time series were then extracted from each parcel, and Pearson’s correlation coefficients between each pair yielded a 1000 × 1000 fMRI connectivity matrix per subject. In order to eliminate negative correlations but avoid disconnection of some parcels, a proportional threshold retaining the top 40% of all connections was applied to each connectivity matrix (see Results for detailed information on this choice of threshold).

Diffusion analysis

Diffusion data were visually inspected for motion, including only data without visible motion. Connectome Mapper software was used to analyze DTI data. Anatomical volumes were registered to B₀ volumes using a rigid body alignment with FLIRT from the FSL toolbox (http://fsl.fmrib.ox.ac.uk/fsl/fslwiki/). Diffusion tensors per voxel were reconstructed using the Diffusion Toolbox (www.trackvis.org/dtk), after which deterministic streamline tractography (angle threshold = 60°) was performed on the entire white matter using 32 random seed points per voxel. Fibers were filtered for length (2–50 cm) and spline filtered for smoothing. Then, an adjacency matrix was generated for each subject by weighing the number of determined connecting fibers by the size of each ROI’s surface area. We also corrected for linear bias toward longer fibers introduced by tractography, as this correction has been shown to lead to reduced intra-subject variability between scans.

Within-module and between-module connectivity

The Brain Connectivity Toolbox and custom-made scripts (Matlab r2012a; Mathworks (Natick, MA, USA)) were used for network analysis. These analyses were performed identically on rsfMRI and DTI connectivity matrices. Newman’s modularity algorithm was used to calculate the optimal modular division into strongly intracerebrally but weakly interconnected modules for each participant, in which each parcel received a single module allegiance, as follows:

\[ Q^w = \frac{1}{|E^w|} \sum_{i,j \in N} \left[ w_{ij} - \frac{k_i^w k_j^w}{l} \right] \delta_{m_i, m_j} \]

in which \( E^w \) is the weight of all links in the network, \( w_{ij} \) is the connection weight between nodes i and j (within the total set of network nodes \( N \)), \( k_i^w \) is the weighted degree of node i, and \( \delta_{m_i, m_j} \) refers to differences in community index between nodes i and j.

Subsequently, connectivity of each parcel within its own module and between several modules was calculated. Within-module connectivity assesses a parcel’s connectivity within its own module; high values indicate importance on the local (in terms of network neighbors, not spatial closeness), segregated level.
where $m_i$ is the module containing node $i$, $k^w_i m_i$ is the weight of all links between $i$ and all other nodes in $m_i$, and $\bar{k}^w(m_i)$ and $\sigma^w(m_i)$ are the respective mean and standard deviation of the within-module weight distribution.

Conversely, weighted between-module connectivity calculates how strongly a node is connected to other nodes outside its own module:

$$y^w_i = 1 - \sum_{m \in M} \left( \frac{k^w_i (m)}{k^w_i} \right)^2$$

in which $y^w_i$ refers to the weighted participation coefficient of node $i$, $M$ is the set of modules $m$ calculated with the modularity algorithm described above, $k^w_i (m)$ is the weight of links between $i$ and all nodes in $m$, and $k^w_i$ is the weight of all links in the network. Nodes with high between-module connectivity link different subsystems of the brain across longer distances and can be termed connector hubs.

Because the solution to the modular subdivision may differ on each run of the algorithm, modularity analysis was run 1000 times, after which values of between and within-module connectivity were averaged.

**Functional DD**

Functional disconnection of the DMN was expected in TLE, with losses of connectivity between its anterior and posterior parts. Therefore, modular connectivity within this functional module was quantified by a DMN disintegration (DD) score, defined here as intramodular connectivity in the anterior part divided by intramodular connectivity in the posterior part of the DMN. DD values around 1 indicate preserved modular DMN dynamics, while deviating values indicate a shift in DMN modular connectivity toward less integrated functioning and more outward connectivity in either of the two DMN components.

**Statistical analysis**

Statistical analysis was performed with PASW Statistics IBM Corp (Armonk, NY, USA) (version 20) and Matlab. Group differences in subject characteristics were tested using Student’s $t$-tests for independent samples and chi-square tests. Group differences in modular connectivity were tested with regression analyses, and were corrected for multiple testing using the false discovery rate (FDR). Covariates entered into all group-level analyses were age, sex, hippocampal volumes, and relative motion.

Within patients, associations between anatomical and functional modular connectomics were tested with regression analyses, as were correlations of multimodal modular connectivity and seizure frequency/duration. Age, sex, hippocampal volumes, motion, lateralization of TLE, and presence/absence of visible lesions on MRI were always included as covariates in these within-patient analyses.

Finally, mediation effects were tested using the INDIRECT PASW statistics plug-in. The presence of mediation signifies that instead of having a direct effect between the independent variable (functional hub connectivity) and dependent variable (seizure frequency/duration); the mediator (anatomical hub connectivity) plays an important role in the association between these two variables. Mediation involved regression analyses to test these direct and indirect effects, after which 95% CIs were calculated for the total indirect effects using bootstrapping (10,000 samples) as an unbiased means of model validity testing. Based on above-mentioned analyses, only significant covariates (age, sex, motion) were taken into account.

Level of statistical significance was set at group-wise $P < 0.05$ for all analyses, taking multiple comparisons into account.

**Results**

**Subject characteristics**

Forty-nine TLE patients and 23 controls participated (Table 1), after exclusion of two eligible patients showing excessive motion during scanning. Thirty-two patients had left-sided TLE (LTLE), whereas 17 had right-lateralized epilepsy (RTLE). LTLE patients had significantly higher seizure frequency (16.0 ± 24.6) than RTLE patients (4.7 ± 7.6; $t(40) = 2.181, P = 0.037$), but these groups did not differ regarding other clinical parameters. Nineteen patients did not show lesions on 3T MRI. Most patients with lesions on MRI had suspected mesial temporal sclerosis (MTS) or cortical dysplasia, with one patient showing a cavernous malformation and one patient having an area of heterotopia. Although none of the patients had undergone surgery before rsfMRI and DTI, information regarding outcome of surgery performed after scanning mostly supports suspected diagnoses. Surgery was performed in 18 of the total 49 patients with a follow-up of 1 year at the time of writing (20 in total), with most (i.e., 14 or 78%) patients being seizure-free at least 1 year after resection of the affected temporal lobe (Engel class I). Two patients had meaningful reductions in seizure frequency 1 year post-
the parieto-occipital module (POM). In patients, benchmark analysis yielded four modules (Fig. 2B), with the DMN+ disconnected into separate anterior and posterior parts (aDMN+ and pDMN+, respectively), as expected and further illustrated in Figure 3. When looking at participants’ individual modular decomposition, all but one control had intact DMN+ (96%), whereas 27 patients (55%) showed disconnection (chi-square $P < 0.001$). Of the total 49 patients, 44 had three (20% or 45%) or four (24% or 55%) modules. Three patients had two modules, whereas two patients had five modules. Patients’ individual modules particularly overlapped less spatially with the pDMN+, as determined by Dice indices (Table 2).

Anatomically, nine modules were found in the healthy benchmark modular connectome, whereas patients’ averaged connectivity matrix yielded seven modules (Fig. 2C and D). There were no significant group differences in individual spatial overlap with the benchmark modules (Table 2).

### Functional hub connectivity

All following analyses took place on participants’ individual modular decomposition and subsequent calculation of hub connectivity. In TLE patients, the DMN+ was characterized by lower within-module connectivity overall, although not significantly after FDR correction (Table 3). Furthermore, the DMN+ showed a shift in between-module hub connectivity from its anterior to its medial posterior parts (Fig. 4). The POM displayed fewer connections to other modules in TLE, but higher within-module connectivity.

Within patients, DD trended toward correlation with seizure frequency when correcting for all covariates (regression B 95% CI $-3.769$ to $45.596$, $P = 0.094$), although none of the covariates (age, sex, TLE lateralization, hippocampal volumes, visible lesion on MRI, motion) were significant. When removing all covariates except age and gender, the beta coefficients were similar but statistical significance improved greatly (regression B 95% CI $3.391$ to $46.630$, $P = 0.025$), suggesting that statistical power was limited when using a number of noninfluential predictors. No associations were present with seizure duration (Table 4), and addition of seizure duration barely changed statistical significance of the association between DD and seizure frequency (regression B 95% CI $-1.533$ to $42.399$, $P = 0.067$). POM hub connectivity was not associated with seizure frequency or duration.

### Anatomical hub connectivity

Patients showed widespread losses of between-module connectivity (Fig. 4). This loss was found in the DMN+ (functionally defined as the patient benchmark aDMN+ and pDMN+), as well as when globally averaging over all modules.
parcels (Table 3), indicating a general phenomenon. Within-module connectivity was not statistically different between groups after FDR correction, whereas it was lower in the averaged pDMN+ in TLE patients. RTLE patients had lower between-module connectivity (0.087 ± 0.04) than LTLE patients (0.162 ± 0.07; regression B 95% CI 1.658 to 5.236, \( P < 0.001 \)). However, both LTLE and RTLE groups' values were lower than controls (0.220 ± 0.03; regression B 95% CI −7.732 to 0.143, \( P = 0.042 \), and regression B 95% CI −7.274 to 4.329, \( P < 0.001 \), respectively).

Within patients, global between-module connectivity was positively correlated with monthly seizure frequency (Table 4). There were no significant effects of age, sex, TLE lateralization, hippocampal volumes, visible lesion on MRI, or motion. It was not associated with seizure duration, and adding duration to the regression model involving seizure frequency did not change results.

**Functional and anatomical hub connectivity and seizures**

In patients, functional DD and anatomical between-module connectivity were positively correlated (regression B coefficient 95% CI 0.171 to 2.482, \( P = 0.025 \), Fig. 5): indicating that lower, more disturbed anatomical between-module connectivity correlated with less dysfunctional DMN+.

There were no significant effects of age, sex, TLE lateralization, hippocampal volumes, visible lesion on MRI, or motion. This association was present in LTLE and RTLE groups separately (TLE lateralization regression B coefficient 95% CI −0.086 to 0.226, \( P = 0.373 \)).

We then tested whether global anatomical between-module connectivity mediated the association between functional DD and seizure frequency. The association between DD and higher seizure frequency proved to be mediated by higher anatomical between-module connect-
Figure 3. Within-module DMN+ connections in patients versus controls. Purple nodes indicate the aDMN+ and pDMN+, blue nodes are the parcels outside of the DMN+. (A) Depicts all within-module connections in healthy controls, (B) displays those within-module connections in TLE patients. aDMN+/pDMN+, anterior/posterior default mode network; TLE, temporal lobe epilepsy.

Table 2. Dice indices between individual and benchmark modules in patients and controls.

<table>
<thead>
<tr>
<th>Benchmark module</th>
<th>Dice index</th>
<th>Group difference</th>
<th>t</th>
<th>P-value</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>M controls (SD)</td>
<td>M patients (SD)</td>
<td>B [95% CI]</td>
<td></td>
</tr>
<tr>
<td>Functional network</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>aDMN+</td>
<td>0.613 (0.0703)</td>
<td>0.607 (0.114)</td>
<td>-0.023 [-1.200 to 0.709]</td>
<td>-0.407</td>
</tr>
<tr>
<td>pDMN+</td>
<td>0.450 (0.143)</td>
<td>0.252 (0.0613)</td>
<td>2.023 [1.393 to 2.653]</td>
<td>6.413</td>
</tr>
<tr>
<td>SMM</td>
<td>0.642 (0.116)</td>
<td>0.356 (0.135)</td>
<td>0.250 [-1.066 to 1.066]</td>
<td>0.612</td>
</tr>
<tr>
<td>POM</td>
<td>0.595 (0.117)</td>
<td>0.660 (0.117)</td>
<td>-0.859 [-1.18 to -0.138]</td>
<td>-2.379</td>
</tr>
<tr>
<td>Anatomical network</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Right lateral motor</td>
<td>0.273 (0.175)</td>
<td>0.182 (0.146)</td>
<td>0.781 [0.196 to 1.366]</td>
<td>2.665</td>
</tr>
<tr>
<td>Medial motor</td>
<td>0.288 (0.169)</td>
<td>0.215 (0.136)</td>
<td>0.445 [-0.192 to 1.081]</td>
<td>4.395</td>
</tr>
<tr>
<td>Left lateral motor</td>
<td>0.295 (0.136)</td>
<td>0.241 (0.169)</td>
<td>0.125 [-0.506 to 0.757]</td>
<td>0.396</td>
</tr>
<tr>
<td>SMA</td>
<td>0.285 (0.189)</td>
<td>0.223 (0.117)</td>
<td>0.441 [-0.214 to 1.096]</td>
<td>1.344</td>
</tr>
<tr>
<td>Left occipital</td>
<td>0.293 (0.212)</td>
<td>0.242 (0.173)</td>
<td>0.231 [-0.282 to 0.744]</td>
<td>0.900</td>
</tr>
<tr>
<td>Right parietal</td>
<td>0.347 (0.233)</td>
<td>0.218 (0.145)</td>
<td>0.664 [0.167 to 1.162]</td>
<td>2.668</td>
</tr>
<tr>
<td>Right occipital</td>
<td>0.327 (0.278)</td>
<td>0.253 (0.183)</td>
<td>0.377 [-0.055 to 0.810]</td>
<td>1.743</td>
</tr>
<tr>
<td>Right frontal</td>
<td>0.201 (0.184)</td>
<td>0.221 (0.149)</td>
<td>-0.002 [-0.610 to 0.606]</td>
<td>0.007</td>
</tr>
<tr>
<td>Left frontal</td>
<td>0.312 (0.231)</td>
<td>0.189 (0.144)</td>
<td>0.621 [0.117 to 1.125]</td>
<td>2.460</td>
</tr>
</tbody>
</table>

All regression models corrected for motion, age, sex, and hippocampal volumes. aDMN+/pDMN+, anterior/posterior default mode network; SMM, sensorimotor network module; POM, parieto-occipital module; SMA, supplementary motor area.

*P < 0.05 (after FDR correction).
tivity (Fig. 6; 95% CI 2.723 to 25.092). Additionally, a mediation model with higher seizure frequency relating to increasing anatomical modular connectivity through higher DD also yielded significant results (Fig. 6; 95% CI 0.0001 to 0.0011).

Role of possible confounders

Age

We controlled for the group age difference by adding this confounder to all analyses. In order to completely rule out that the difference in age between patients and controls caused our findings, we also repeated group analyses on a subsample consisting of controls and the 23 youngest patients (mean 25.9 ± 5.14 years). This analysis yielded predominantly identical results, apart from an increased P-value of the association between functional DD and seizure frequency (beta coefficient 95% CI −0.379 to 129.08, P = 0.051), possibly due to reduced statistical power in this smaller sample. More importantly, the investigation of the association between anatomical and functional modular connectivity within patients is separate from controls and thus not influenced by this group difference in age.

Subject motion

Since group differences in motion may influence connectivity and network findings, and patients showed higher motion than controls in our study, we also repeated all analyses using a subsample of patients with motion equal to controls (patients n = 32, both groups relative motion mean 0.08 mm, range [0–0.15] mm, two-tailed Student’s t-test 95% CI 0.020 to 0.017, P = 0.862). Results were identical, apart from the association between DD and seizure frequency, which lost significance but remained a statistical trend when taking age and sex into account (regression B 95% CI 1.953 to 65.74, P = 0.064).

AED use

The influence of anti-epileptic drugs (AEDs) on connectivity and networks is largely unknown. Furthermore, most patients in our study used multiple AEDs with highly variable AED combinations, rendering controlling for this factor difficult. We did test whether the number of different AEDs used (monotherapy vs. polytherapy as well as number of AEDs from 1 to 4) influenced our results. This proved not to be the case, and neither variable was ever significant as a covariate.

Functional connectivity threshold

Another common confounder in functional network analysis is the choice of functional connectivity threshold in rsfMRI, as negative correlations are incompletely understood physiologically. We retained the 40% highest connections, because this proportional threshold signified the highest number of connections (and thus information) we were able to retain without also including negative correlations.
tive correlations. Furthermore, using a proportional threshold prevents a priori interindividual differences causing connectivity network topology differences. In order to investigate the robustness of our results with respect to choice of threshold, we repeated our analyses using 20% and 30% of the connections, but these analyses did not yield different results.

**Functional modularity methods**

Functional modularity analysis usually results in a resting-state network structure comparable to other methods of dividing the brain into meaningful subsystems. In order to compare to other commonly used methods of resting-state analysis, we replicated our data-driven results with a seed-based approach. The averaged control connectivity matrix was used to seed each resting-state network, and all connections with Pearson’s rho >0.3 were included per module. These analyses yielded smaller networks and more significant results in general, but findings in terms of differences in module overlap between patients and controls did not change.

![Figure 4](image.png)

**Figure 4.** Group differences in modular connectivity. All displayed results are significant with \( P < 0.05 \) after false discovery rate (FDR)-correction for multiple testing and correction for covariates. (A) Displays differences in functional between-module connectivity in patients as compared to controls. Warm colors indicate higher connectivity in patients, cool colors signify higher connectivity in controls. (B) Indicates functional within-module connectivity in patients versus controls, whereas (C) shows differences in regular functional connectivity per parcel. In (D), anatomical between-module differences are depicted. There were no significant parcel-based differences between groups in within-module or regular anatomical connectivity after correcting for confounders and multiple testing.


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Discussion

TLE patients have disturbed functional and anatomical connectomes, with distinct alterations in hub connectivity characterizing both modalities. More importantly, functional and anatomical modular connectomics interact to influence seizure burden. As hypothesized, the (extended) functional DMN broke down into separate anterior and posterior parts in TLE, corroborating previous studies. We show that both the aDMN and pDMN lose internal communication, but that particularly the pDMN gains pathological long-range connectivity to other functional modules in TLE. This DD correlates with higher seizure frequency, but not duration.

In computational epilepsy models, changes in specific functional connection types and particularly hub-associated connectivity greatly impact seizure vulnerability. Network segregation into more independent modules is thought to be a mechanism for containment of (pathological) activity, suggesting that increased functional connectivity between modules leads to higher seizure frequency. In epileptic rodent medial temporal lobe, areas with high long-range hub connectivity are responsible for generation of seizures that spread throughout the entire hippocampus. We have shown positive correlations between seizure frequency and functional between-module connectivity of the tumor in glioma patients. Our results concerning the shift of within-module to between-module DMN hub connectivity and its correlation with seizure frequency in TLE corroborate these studies.
Why does this shift occur, and why is it specific to the DMN? In healthy brains, DMN areas form important functional hubs,44,45 with efficient connectivity in the precuneus, posterior cingulate, and inferior parietal cortices associated with cognition and behavior.46,47 Modeling brain activity on anatomical networks shows that hubs are more vulnerable to functional dysfunction exactly because of their high use.48 This may render the DMN the go-to spot for neurological diseases in general. For instance, Alzheimer’s disease is accompanied by decreases in functional DMN hub functioning, with pathological amyloid deposition and atrophy spatially overlapping the DMN.44 This apparent hub preference for dysfunctioning combined with high connectivity to all other subsystems may lead to global connectomic impairment when the DMN becomes implicated.49,50 We term this hypothetical sequence of events a “catastrophic connectomic cascade”.

Our study does not address the mechanism underlying this cascade of connectomic changes in TLE. Connectivity between the ipsilateral medial temporal lobe and the rest of the DMN may relate to either poorer51 or better52 memory functioning in TLE, depending on the study. Increased connectivity to and within the contralateral DMN has been linked to better cognitive performance as a “compensatory mechanism”.51–54 Speculatively, increased DMN connectivity relates to preserved cognitive functioning in TLE, although this increase is also accompanied by an increase in seizure frequency. Interestingly, increased within-module connectivity but decreased between-module connectivity for dysfunctional combined with high connectivity to all other subsystems may lead to global connectomic impairment when the DMN becomes implicated.49,50 We term this hypothetical sequence of events a “catastrophic connectomic cascade”.

Anatomically, TLE patients displayed global losses of between-module connectivity. Previous studies have shown decreased white matter integrity,7,61 with local increases in clustering and efficiency.8,9 Global loss of between-module connectivity seems evident from earlier and current work.8 Corroborating modeling studies,43 this sign of increased modular segregation was associated with diminished seizure frequency, suggesting that an anatomically more compartmentalized connectome is favorable for seizure vulnerability. A problem with this interpretation is that patients with higher seizure frequency were more comparable to healthy controls in terms of between-module connectivity.

Again, the effect of time on the anatomical connectome may relate to these findings. The positive association between seizure frequency and anatomical between-module connectivity was not affected by seizure duration. However, seizure duration and frequency were correlated, which makes distinction between these two factors difficult. Almost certainly, anatomical connectomics in TLE are related to dynamics of the disease, albeit not on a linear time scale. Instead of viewing anatomical connectomics as an endpoint of gradual change, it could be at any of a range of intermediate states: patients may have decompensated first, after which compensatory change could have occurred. Future longitudinal investigations are necessary to further study these dynamics.

We replicated correlations between anatomical and functional connectomics in TLE,5,14 but specified which types of multimodal hub connectivity are correlated while adding important insights about associations with seizure frequency. The association between DD and increased seizure frequency was mediated by higher anatomical between-module connectivity. However, higher seizure frequency also related to higher anatomical between-module connectivity through the mediating effects of modular DD. This indicates a vicious circle of seizures, disturbed DMN integrity and abnormal modular anatomical connectomics. The unpredictable, nonlinear transition from local anatomical damage to global connectomic dysfunction has also been shown in modeling work,62 further underlining the necessity of viewing TLE as a highly
dynamical disease in which anatomy and function need to be taken into account as separate but interacting entities. Of course, these mediation analyses are statistical in nature, and our cross-sectional design does not allow for investigation of causality in any way.

Where do these results leave us in terms of clinical care? Interestingly, normalization of connectivity within the DMN after surgical intervention in TLE is positively correlated with memory outcome\textsuperscript{52}, supporting the view that (restoration of) DMN integrity is pivotal in TLE. Combined with our results, hub connectivity signature may be a sensitive predictor of functioning in terms of both cognition and seizure burden. There may also be more direct methods of using connectomics to patients’ benefit: perturbing the brain by means of magnetic or electric stimulation may alter DMN connectomics (among others), hereby improving functioning.\textsuperscript{53} Indeed, several studies report improvement of symptoms in epilepsy patients after brain stimulation.\textsuperscript{64} Future investigations are needed to assess the effects of stimulation on DMN hub connectivity.

Some study limitations should be kept in mind. First, there were some confounding differences between patients and controls (age, rsfMRI sequence, relative motion). We have taken every possible measure to minimize effects of age and motion on our results. The impact of sequence could not be mitigated, although its influence may be limited.\textsuperscript{42} More importantly, the association between anatomical and functional hub connectomics and its clinical implications was determined within patients and is thus unaffected. Second, network analysis can be done in several ways. Using a proportional threshold diminishes the possibility of overall differences in connectivity between groups leading to network topology differences, supported by the robustness of our results when using more strict thresholds. Third, our modularity analyses placed both medial and lateral areas into the same module. Although these results are comparable to studies using the same modularity algorithm,\textsuperscript{65} they differ slightly from others. Fourth, although some studies (generally with smaller sample size) report connectomic differences between RTLE and LTLE patients,\textsuperscript{4,66} we only found significantly lower anatomical between-module connectivity in RTLE patients. Drug-refractory epilepsy TLE may only represent a subgroup of TLE, therefore potentially causing a selection bias in our study. Also, right and left TLE may be associated with different clinico-pathological features. In our study, RTLE patients had significantly lower seizure frequency, which prevents us from drawing definite conclusions regarding the influence of lateralization alone on connectomics. However, lateralization being a nonsignificant factor in almost all analyses suggests that the results described are common effects of TLE, regardless of affected hemisphere.

In conclusion, TLE is a multimodal connectomic disease, which impacts anatomical and functional hub connectivity differently. Shifts in functional hub connections from within to outside the DMN, an overall loss of integrative anatomical communication, and the interaction between these two increase seizure frequency.

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Conflict of Interest

Dr. Reinsberger reports grants from Epilepsy Foundation, during the conduct of the study; other from Sleep Med Inc., outside the submitted work. Dr. Douw reports grants from Dutch organization for research (NWO) Rubicon grant, during the conduct of the study.

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