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Citation

Published Version
doi:10.1097/MD.0000000000005410

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Single injection protocol for coronary and lower extremity CT angiographies in patients suspected for peripheral arterial disease

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Abstract
To evaluate the feasibility of a single injection protocol for coronary CT angiography (CTA) and lower extremity CTA in patients suspected for peripheral arterial disease (PAD).

This prospective observational study included a total of 103 patients who showed an ankle brachial index <0.9 and underwent the single injection protocol for coronary and lower extremity CTA. All CTAs used iodinated contrast (weight × 0.06 mL/s × 20 seconds). A prospective Electrocardiogram (ECG)-gated coronary CTA was performed, followed by helical lower extremity CTA beginning 9 seconds after coronary CTA. Using catheter angiography as reference standard, diagnostic ability of CTA was evaluated.

The mean total volume of iodinated contrast used was 70 ± 14 mL. Contrast opacification in the superficial femoral artery was adequate (408 ± 97 Hounsfield Units [HU]) and PAD was detected in 72.8% (75/103). The estimated radiation doses for lower extremity and coronary CTA were 3.6 ± 1.2 and 5.5 ± 4.5 mSv. A significant coronary stenosis was detected in 47 patients (45.6%). Coronary CT image quality was recorded as excellent in 86.4%, acceptable in 11.7%, and unacceptable for 1.9%. Contrast opacification within the superficial femoral artery was adequate in all cases while 27.2% needed an additional scan below the calf to capture the contrast bolus arrival in the smaller lower extremity vessels. Segment based sensitivity, specificity, positive, and negative predictive values were 57.3%, 97.9%, 73.8%, and 95.9% for the coronary CTA, and 63.4%, 91.5%, 76.3%, and 85.3% for peripheral CTA.

A single injection protocol for coronary CTA and lower extremity CTA is feasible with a relatively small volume of iodinated contrast.

Abbreviations: ABI = ankle brachial index, Bpm = beats per minute, CAD = coronary artery disease, CNR = contrast to noise ratio, CTA = CT angiography, DLP = dose length products, HI PAA = health insurance portability and accountability act, HU = hounsfield unit, LMT = left main trunk, PAD = peripheral artery disease, ROI = region of interest, SNR = signal to noise ratio.

Keywords: coronary CT angiography, iodinated contrast media, lower extremity CT angiography, radiation exposure

1. Introduction
Atherosclerosis is a systemic process with high morbidity and mortality that affects multiple organ systems.[1] Patients with hypertension, diabetes, dyslipidemia, smoking, obesity, and physical inactivity are more prone to peripheral artery disease (PAD) and coronary artery disease (CAD).[2] The estimated prevalence of CAD among patients with PAD ranges from 28% to 72% with the higher prevalence of left main and multi-vessel coronary artery disease.[3,4] On the other hand, the prevalence of previously unrecognized PAD is 15% in symptomatic CAD.[5] For patients with PAD, the all-cause mortality is 3.1 times higher than the non-PAD patients, with 6.6 times higher risk of death due to CAD.[6]

Given the concomitant presence of PAD and CAD and the high overall expenditure associated with diagnosis and management,[7] a noninvasive combination study would be desirable for those patients who require examination of both vascular territories. Previous attempts at detecting CAD in patients with PAD have focused on invasive catheter angiography.[3,4,8] Invasive catheter angiography is expensive, has a higher radiation dose than CT, and has a 1% to 2% complication rate.[9] The role of CT angiography (CTA) for the assessment of the coronary arteries and the lower extremity arteries independently has been well established.[10-13] Furthermore, CT hardware technologies enable faster imaging with larger and faster z-axis coverage, thereby proving advantageous in both coronary and peripheral vascular imaging.[14,15] Thus, we hypothesized that it may be technically feasible to obtain combined examinations for both peripheral and coronary vasculature in a single contrast injection and designed a study which purpose is to evaluate the feasibility of such a combined CTA examination.
2. Methods

2.1. Study population

This Health Insurance Portability and Accountability Act (HIPAA)-compliant prospective observational study was approved by the institutional review board of the single institution. Informed consent for undergoing test and the use of images for research was obtained from all patients. During the period from January 2010 to May 2013, 273 patients underwent the single injection protocol for coronary CTA and lower extremity CTA. The inclusion criteria were patients admitted with suspected peripheral arterial disease symptoms prompting further assessment for cardiac disease. After excluding patients with an Ankle Brachial Index (ABI) >0.9 (n=33) and those with a known history of CAD (n = 137), a total of 103 patients were included in analyses (Table 1).

2.2. Imaging protocols

2.2.1. Coronary CTA. Axial coronary CTA was obtained using a first generation 320 × 0.5mm detector-row scanner (Aquilion ONE operating on the v4.51 software platform, Toshiba Medical Systems Corporation, Tochigi-ken, Japan) with a 0.35 second gantry rotation time.[16] The craniocaudal field of view was tailored to the smallest region (10 cm, 12 cm, 12.8 cm, or 14 cm) that encompassed the entire heart. The default kV of 120 was increased to 135 when the maximum tube current (580mA) was reached. Lower kV was not used because the coronary plaque area would not be clearly depicted coronary artery walls on curved multiplanar reformatted views and images orthogonal to the center line were free of motion artifacts. “Acceptable” images had small motion artifact and saline injection rates were calculated by multiplying the individual patient’s mass in kilograms by 0.06 mL per second.

Patients with an average heart rate greater than 60 beats per minute (bpm) and no contraindication to beta-blocker received 2.5 mg atenolol per orally on the evening prior to the examination. Additionally, heart rate control with a target of 60 bpm or less was achieved using intravenously injection of 2 to 10mg propranolol before the data acquisition. The prospective ECG gating acquisition strategy, that is, number of scan beats and the target phase (mid-diastolic or end-systolic), was determined by the heart rate measured during the breath-hold exercise. An arrhythmia rejection algorithm was applied in image acquisition.[17]

2.2.2. Lower extremity CTA. The same hardware was used in helical acquisition mode using the central 64 × 0.5 mm detectors. The gantry rotation time was 0.35 second and the beam pitch was 0.65. The craniocaudal range extended from the upper pole of the kidneys to the mid lower legs. The tube voltage was 120kV and the tube current was modulated according to the patient’s body habitus (by the Volume EC). The manufacturer iterative reconstruction algorithm (AIDR3D) was used (set to “mild”) and images were reconstructed with the FC13 kernel. The target image quality level (SD noise level) was 8.

For all the studies, image acquisition began at a fixed time of 9 seconds after the coronary CTA was completed. If the contrast had not reached to lower extremity arteries on completion of lower extremity CTA acquisition, an immediate re-scan was performed only for necessary regions, without an additional injection of contrast material.

2.3. Image reconstruction

For a coronary CTA, half-scan image reconstruction was performed for the patients imaged in one heartbeat while additional segmental image reconstructions were performed for 2 or more beat scans. Axial reconstructions were performed at 0.3 mm interval for those cardiac phases with the least motion artifact as determined by the attending physician. For a lower extremity CTA, images were reconstructed at 1.0 mm slice thickness. All the reconstructed images were subsequently interpreted using a 3D image post-processing workstation (Zio M900, Ziosoft, Tokyo, Japan).

2.4. Coronary image quality assessment

The image quality of coronary CTA was determined by (Comment 2) a consensus reading of three imagers: two experienced attending cardiovascular physicians plus an experienced CT technologist, all of whom were unaware of the clinical data. “Excellent” images had clearly depicted coronary artery walls on curved multiplanar reformatted views and images orthogonal to the center line were free of motion artifacts. “Acceptable” images had small motion artifact considered acceptable for confident diagnoses. “Unacceptable” images had at least one coronary segment with a 2 mm coronary diameter, which was considered not useful for clinical interpretation (Fig. 1). This group also included patients with unacceptable images due to incomplete breath-hold, insufficient temporal resolution, poor contrast opacification, incorrect imaging scan range, and misalignment.

(Comment 2) To objectively evaluate the image quality, region-of-interest (ROI) measurements of mean and standard deviation Hounsfield Units (HU) on axial images were obtained in the left main trunk (LMT) and in the fat tissue around the LMT.

Table 1

<table>
<thead>
<tr>
<th>Patient characteristics.</th>
<th>N = 103</th>
</tr>
</thead>
<tbody>
<tr>
<td>Gender (% of male)</td>
<td>68.0%</td>
</tr>
<tr>
<td>Age (years)</td>
<td>73.1 ± 9.8</td>
</tr>
<tr>
<td>Height (cm)</td>
<td>159.5 ± 9.1</td>
</tr>
<tr>
<td>Weight (kg)</td>
<td>56.5 ± 12.0</td>
</tr>
<tr>
<td>Body mass index</td>
<td>22.9 ± 3.8</td>
</tr>
<tr>
<td>Ankle/brachial index</td>
<td>0.83 ± 0.22</td>
</tr>
<tr>
<td>Right</td>
<td>0.77 ± 0.23</td>
</tr>
<tr>
<td>Minimum</td>
<td>0.67 ± 0.18</td>
</tr>
<tr>
<td>Chest symptoms</td>
<td></td>
</tr>
<tr>
<td>Typical angina</td>
<td>8.7%</td>
</tr>
<tr>
<td>Atypical angina</td>
<td>33.0%</td>
</tr>
<tr>
<td>Non-anginal chest pain</td>
<td>4.9%</td>
</tr>
<tr>
<td>Asymptomatic</td>
<td>53.4%</td>
</tr>
<tr>
<td>Hyperlipidemia</td>
<td>68.9%</td>
</tr>
<tr>
<td>Total cholesterol</td>
<td>193.4 ± 40.3</td>
</tr>
<tr>
<td>Triglyceride</td>
<td>160.6 ± 116.2</td>
</tr>
<tr>
<td>LDL-cholesterol</td>
<td>120.8 ± 52.4</td>
</tr>
<tr>
<td>Family history of coronary artery disease</td>
<td>19.4%</td>
</tr>
<tr>
<td>Hypertension</td>
<td>74.8%</td>
</tr>
<tr>
<td>Diabetes</td>
<td>35.9%</td>
</tr>
<tr>
<td>History of stroke</td>
<td>18.6%</td>
</tr>
<tr>
<td>Smoking</td>
<td>32.0%</td>
</tr>
</tbody>
</table>

LDL = low-density lipoprotein.
Signal-to-noise ratio (SNR) was calculated at LMT by dividing the absolute mean value within the ROI by the standard deviation. Contrast-to-noise ratio (CNR) was calculated by the difference in mean HU between the LMT and fat divided by the standard deviation in the LMT. In 3 out of 103 cases, axial CT images were not available at the time of analysis and thus the mean SNR and CNR were calculated in the remaining 100 cases.

2.5. Contrast opacification of lower extremity arteries

A circular ROI was placed in the superficial femoral artery by an experienced cardiovascular imager to evaluate contrast opacification. When re-scan was performed due to the delayed arrival of the contrast, ROI analysis was performed using the second image dataset.

2.6. Stenosis evaluation

2.6.1. Coronary CTA. Coronary artery stenosis was evaluated on the CT images by the consensus reading of two cardiovascular imagers who were unaware of clinical findings. The coronary system was divided into the American Heart Association 16 segment model.[18] On the 0.3 mm short axis images, the stenosis was divided into the American Heart Association 16 segment model.[18] On the 0.3 mm short axis images, the stenosis was estimated and considered significant if the luminal stenosis was >50% of the diameter.

2.6.2. Lower extremity CTA. Stenosis of the iliac/lower extremity arteries was evaluated on CT images by the consensus reading of two cardiovascular imagers who were unaware of clinical findings. The arterial system was divided into iliac, femoral, and arteries of the lower leg. On the 1.0 mm short-axis and long-axis images, the stenosis was estimated and considered significant if the luminal stenosis was >50% of the diameter.

2.7. Estimated radiation dose

Radiation doses of CTA were estimated using the dose length products (DLP). The conversion factor used was \( k = 0.014 \) for the coronary CTA, and, 0.015 for abdominal/pelvic regions and 0.0008 for extremity regions for lower extremity CTA.

2.7.1. Coronary catheter angiography. Based on the coronary CTA findings and a clinical assessment, coronary catheter angiography was performed within 2 weeks after coronary CTA in 69 patients. After pretreatment with 200 mg of aspirin and intravenous bolus of unfractionated heparin to maintain a therapeutic activated clotting time over 250 seconds, intracoronary contrast (Omnipaque 350, Daiichi Sankyo Campany, Tokyo, Japan) was injected (ACIST CVi, Acist Medical Systems, Minneapolis, MN) at 2.5 mL/s and multiple projections at a frame rate of 15 per second were acquired using a single plane angiography system (INFX 8000 V, Toshiba Medical Systems Corporation, Tochigi-ken, Japan).

2.7.2. Lower extremity catheter angiography. Based on the CTA findings and clinical assessment, lower extremity catheter angiography was performed within 2 weeks after CTA in 62 patients. After pretreatment with intravenous bolus of unfractionated heparin (5000–8000IU) to maintain a therapeutic activated clotting time over 250 seconds, a total of 5 to 9 mL iodinated contrast (Omnipaque 350, Daiichi Sankyo Campany, Tokyo, Japan) was manually injected. A single anterior-posterior projection at a frame rate of 15 per second was acquired using a single plane angiography system (INFX 8000 V, Toshiba Medical Systems Corporation, Tochigi-ken, Japan).

2.8. Clinical data collection

For each patient, a retrospective review of the medical record was performed to collect clinical data.

2.9. Statistical analysis

Continuous values were expressed with mean and standard deviations. Categorical values were presented in percentage. Test characteristics were calculated as sensitivity, specificity, positive predictive value, and negative predictive value with 95% confidence interval, with catheter angiography as reference standard. (Comment 1). All the analyses were performed using STATA version 10.1 (Stata Corp., College Station, TX).

3. Results

The population and clinical characteristics are summarized in Table 1. Hypertension was the most common risk factor and was seen in up to 75% of the patient population. The mean total volume of the iodinated contrast used for CTA was 70 ± 14 mL.

3.1. Coronary CTA

CT imaging characteristics are summarized in Table 2. One and two heart-beat scans were performed in 57 cases (54.4%) and in 42 cases (40.8%), respectively. Image quality was recorded as “unacceptable” for only two studies (1.9%) due to motion artifact. (Comment 2) The mean SNR and CNR were 24.0 ± 7.6 and 27.7 ± 8.7, respectively. The estimated mean radiation dose for coronary CTA was 5.8 ± 4.4 mSv.

Although 53.4% (55/103) of patients had no cardiac symptoms at the time of CT acquisition (Table 1), a significantly stenotic segment was detected by a coronary CTA in 45.6% of the population. Among the remaining, 13 patients had at least one segment that was not evaluable for luminal stenosis due to...
severe calcification. A percutaneous coronary intervention in the form of angioplasty was performed in 43 patients (41.7%).

3.2. Lower extremity CTA

Among the 103 studies, 28 patients (27.2%) needed an additional scan below the calf to capture the contrast bolus arrival in the smaller lower extremity vessels. Contrast opacification within the superficial femoral artery was adequate (mean ± SD: 408 ± 97 HU) with all cases having the CT attenuation number above 220 HU (range: 221–633 HU). The estimated mean radiation dose for lower extremity CTA was 3.6 ± 1.2 mSv. Significant luminal stenosis was detected in at least one artery in 75 patients (72.8%). Figure 2 shows representative coronary and lower extremity CTA images.

3.3. Diagnostic ability

Regarding diagnostic ability of CTA, in all patients with coronary catheter angiography (n = 69), all coronary segments (total n = 1173) were analyzed independent of image quality. For lower extremity vessels, total of 372 segments were evaluated in 62 patients who underwent lower extremity catheter angiography. The test characteristics of CTA (with 95% confidence interval) in the detection of stenosis were calculated by using catheter angiography as reference standard (Table 3).

4. Discussion

PAD is common,[19] and atherosclerosis leading to CAD likely represent different clinical forms of the same pathophysiologic process.[20] CAD is the leading cause of postoperative mortality in patients who undergo surgery for PAD[21] and the two processes often coexist, it becomes important to recognize and exclude CAD for preintervention/surgical risk stratification.

We report CAD in approximately 45% of patients with PAD, who underwent combined CTA for coronary and lower extremity circulation with reported prevalence varying widely.[14,22,23] The CTA accuracy is based on reference standard catheter angiography, and lower extremity imaging have a high sensitivity and positive predictive value on a per patient basis. Although patients with PAD had a high prevalence of CAD and thus the diagnostic values of coronary CTA are difficult to be interpreted in accordance with those in so-called “suspected CAD” population, high-negative predictive value in the per-segment analysis is in keeping with the individual literatures. To our knowledge, there is no prior data in the literature regarding a combined protocol with reference standard catheter based angiography.

CAD is often more severe and has a poor outcome in the presence of PAD when compared with the general population,[13,14] Nearly 42% of patients in this study required some form of coronary intervention, confirming this association. Also, the severity of CAD increases with more severe PAD.[19,23] ABI is widely used as a quantitative measure to determine the presence and severity of PAD.[24] While most test characteristics are high for ABI, the sensitivity varies (15–79%) and is lower in elderly individuals and patients with diabetes.[25] Imaging is essential as computed tomography (CT) or magnetic resonance imaging can identify the location and severity of disease and the decision to choose between surgical and endovascular management can usually be made non-invasively using these cross-sectional imaging modalities.

A combined CAD and PAD examination that uses the same bolus of contrast material may be desirable for a subset of patients with clinically suspected coexisting PAD and CAD. Coronary revascularization for significant CAD, before the PAD intervention/surgery results in good long-term outcomes supporting the idea that aggressive management of CAD is required to improve patient outcomes.[13,24] It has been shown in prior studies that simultaneous coronary bypass and peripheral artery bypass surgery may be safe and feasible in PAD patients with asymptomatic CAD.[23] We report a protocol that uses wide-area detector CT to accomplish the goal of simultaneous imaging of both the anatomic territories using single time injection. Other hardware platforms can likely be used as well, but we believe that none has been reported to date. Had coronary CTA and lower extremity CTA were performed separately, more iodinated contrast would be needed. We calculated the estimate of 97 ± 20 mL by using the following equation: body weight × 0.04 mL/s × 25 seconds for lower extremity CTA + body weight × 0.06 mL/s × 11 seconds for coronary CTA. The high negative predictive value of coronary CTA also makes it highly effective noninvasive alternative to invasive coronary catheter angiography for the exclusion of obstructive coronary artery stenosis in PAD patients.

The estimated radiation doses for lower extremity and coronary CTA were 3.6 ± 1.2 and 5.5 ± 4.5 mSv, respectively. Thus, the dose profile is comparable or less than the sum of individual exams[27,28] and given the age and co-morbidities, this level of exposure is considered to be of negligible risk for a fatal radiation induced malignancy. The dose estimates also include the roughly one-quarter of patients for whom a second lower extremity exposure was required to optimize contrast enhancement in the leg. It is hard to estimate the best time delay based on
the current data since we used the fixed delay time of 9 seconds, but a few more seconds would be necessary so that the contrast reach to the whole lower extremity arterial tree in the majority of the cases. Improvement of the scan timing would further lower the total radiation exposure.

There are several limitations to our study. First, all patient data were acquired in a single center, which may need external validation. Second, due to limited follow up, the assessment of exact prognostic benefit in actual patient outcome was not possible. Third, we could not calculate the actual cost benefit

| Test characteristics of the CTA studies using catheter angiography as reference standard. |
|---------------------------------------------|-------------|-------------|-------------|
| Sensitivity | Specificity | Positive predictive value | Negative predictive value |
| Coronal CTA  | 57.9% (48.0–67.4) | 97.9% (96.9–98.7) | 73.8% (63.1–82.8) | 95.9% (94.5–97.0) |
| Patient-based (n=69) | 76.6% (62.0–87.7) | 77.3% (54.6–92.2) | 87.6% (73.6–95.9) | 60.7% (40.6–76.5) |
| Lower extremity CTA | 63.4% (53.8–72.3) | 91.5% (87.4–94.6) | 76.3% (66.4–84.5) | 85.3% (80.5–89.2) |

CTA = CT angiography.

Table 3

1 The number of the negative was 1.
using this protocol compared with the conventional approach for managing the combined coexisting PAD and CAD. The data on sensitivity and specificity regarding stenosis detection may be influenced by verification bias since not all patients received invasive angiography. Long term prospective studies are required in the future using this protocol will be helpful to establish this protocol in actual clinical practice. (Comment 3) Finally, although we used smaller volume of iodinated contrast compared with the simulated situation where coronary CTA and lower extremity CTA are performed separately, recent studies have shown that the contrast amount can be reduced to approximately 20mL for coronary CTA when using low kVp and iterative reconstruction. Further study is warranted to test if these new techniques can also reduce the contrast volume for the single injection protocol.

In conclusion, we report a single contrast injection CTA protocol to assess both the coronaries and the lower extremity runoff. The high degree of correlation between the CT imaging and catheter angiography in a subset of our patient population suggests that this strategy can be used for patients who require both studies and for whom additional contrast material may be concerning. Patients without significant coronary stenosis can, in theory, avoid invasive angiography and those with significant CAD can go for either intervention or surgery based on its results before PAD intervention. The adoption of such diagnostic strategies using combined CTA protocols warrants further investigation.

References


