Characterization of Individual Polynucleotide Molecules Using a Membrane Channel

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Characterization of individual polynucleotide molecules using a membrane channel

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ABSTRACT We show that an electric field can drive single-stranded RNA and DNA molecules through a 2.6-nm diameter ion channel in a lipid bilayer membrane. Because the channel diameter can accommodate only a single strand of RNA or DNA, each polymer traverses the membrane as an extended chain that partially blocks the channel. The passage of each molecule is detected as a transient decrease of ionic current whose duration is proportional to polymer length. Channel blockades can therefore be used to measure polynucleotide length. With further improvements, the method could in principle provide direct, high-speed detection of the sequence of bases in single molecules of DNA or RNA.

Measurement of ionic current passing through single ion channels in biological membranes or planar lipid bilayers is routine in neurobiology and biophysics (1, 2). Although most such channels undergo voltage- or ligand-dependent gating (3, 4), several relatively large ion channels, including Staphylococcus aureus α-hemolysin (5, 6) and the mitochondrial voltage-age-dependent anion channel (7, 8), can remain open for extended periods, thereby allowing continuous ionic current to flow across a lipid bilayer (9, 10). We reasoned that a transmembrane voltage applied across a continuously open channel of appropriate size should draw polyionic DNA or RNA molecules through the channel as extended linear chains whose presence would detectably reduce or block normal ionic flow. Such blockages should make it possible to use single channel recordings to characterize the length and, possibly, other characteristics of the polymer.

Random coil polymers have previously been used to investigate channel pore dimensions (8) and single channel current recordings show that small poly(ethylene glycol) polymers partition into channels formed by alamethicin (11) or S. aureus α-hemolysin (12, 13). Recent investigations show that proteins can also traverse a lipid bilayer by moving through protein translocating channels, presumably as unfolded, extended chains (14–18). While translocating a protein, such channels are electrically silent; they regain their ion permeability only after the translocating polypeptide has been cleared from the channel (18). The ionic conductance of large nuclear pore complexes is similarly reduced during translocation of transcription factors, although in this case the macromolecules are assumed to move through the nuclear pore in a folded state (19, 20).

To determine whether nucleic acid polymers can be detected by single channel measurements, S. aureus α-hemolysin was used to form a single channel across a lipid bilayer separating two buffer-filled compartments (21). The α-hemolysin monomers spontaneously insert into lipid bilayers (9) and assemble to form heptameric transmembrane channels (6) that are 2.6 nm in diameter (L. Song, M. R. Hobaugh, C. Shustak, S. Cheley, H. Bayley, and J. E. Gouaux, personal communication). Channels with this dimension should be sufficiently large to accommodate the diameter of an extended, single-stranded polynucleotide.

MATERIALS AND METHODS

Conductance Measurements. A solvent-free bilayer membrane of diphytanoyl-PC (Avanti Polar Lipids) was formed across a ~0.1-mm-diameter orifice in a 25-μm thick Teflon partition separating two buffer filled compartments (ref. 23, patterned after ref. 21) each containing 1.5 ml of 1 M KCl, 5 mM Hepes (pH 7.5). α-Hemolysin channels were reconstituted into the membrane by adding less than 1 μg of α-hemolysin to the compartment we designated as cis. A single channel usually formed within 5 min. To prevent further channel incorporation, the cis compartment was flushed extensively with fresh buffer solution. The current was converted to voltage and amplified by either an Axopatch 200A (Axon Instruments, Foster City, CA) or a Dagan 3900A patch clamp amplifier (Dagan Instruments, Minneapolis). The signal was filtered at less than 3/8 the sampling rate, which was typically 64,000 samples/sec, using a Frequency Devices (Haverhill, MA) low pass Bessel filter. Unless stated otherwise, the data was digitized using a National Instruments (Austin, TX) AT-MIO-16-X 16-bit board using programs written in LAB WINDOWS/ CVI (National Instruments). The bilayer apparatus was shielded from electric and magnetic noise sources using a μ-metal box (Amuneal, Philadelphia).

Polynucleotides. For most of our experiments we used polyuridylic acid (poly[U]) because this homo-polynucleotide has minimal secondary structure or base pairing (24) that might interfere with translocation of the polymer. Fractions of the poly[U] (Sigma), prepared with polynucleotide phosphorylase, were size selected by elution from agarose after fractionation by electrophoresis in the presence of formaldehyde. All DNA was synthesized using standard phosphoramidite methods. Although the sequence of the 150-nt DNA (CT-CACCTATC CTTCCACTCA TTITCCTTAA CCATT-TCATT CACCCATCTC TTCACTCCAT CTACATCCTAC TACATCCAT CACTTACCAT CACTCCCTACT ATCTAT-CTATC ATCAATC CAA TCACATCCAT ACCTCCATAC TACATCCAC TACATCCACA CACTCCATAC) was designed to minimize base pairing expected in the nondenaturing conditions we used, this polymer exhibited a larger proportion of long-lived blockades than did the homopolymers. Many of these blockades required clearing by brief polarity reversal. The 120-nt DNA for competitive PCR contained the same sequence as the 150-nt molecule but lacked residues 97–126. Double-stranded DNA, designed to be amplified by PCR using the same primers as the 150-nt single-stranded DNA, was made by mixing and annealing a synthetic 100-nt sense strand with its 100-nt antisense strand. The 100-nt sense strand contained the same sequence as the 150-nt molecule but lacked residues 49–98.

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**PCR Analysis and Blockade Counts.** Competitive PCR analysis (25) was performed after amplification (26) to avoid the plateau phase. To prevent DNA loss by adsorption to the trans chamber walls, 55 μg/ml of carrier poly[U] was added to the trans chamber when DNA was to be harvested for PCR analysis. The PCR products were resolved on a 15% (total monomer) acrylamide gel and stained with SYBR Green I (Molecular Probes) for densitometry. In experiments with 1–8 channels, the number of blockades in peak 2 + peak 3 was determined by counting individual blockades during several 5-min sampling periods throughout the experiment; in the experiment with 40 channels, the number of blockades was estimated by multiplying (peak 2 + peak 3 rate observed with one channel) × (number of channels in the membrane) × (time of experimental voltage application).

**RESULTS AND DISCUSSION.**

In the absence of polymer, applying a potential of −120 mV (cis side negative) resulted in single channel currents that were free of transients (Fig. 1). Following the addition of poly[U] to the cis chamber, numerous short-lived current blockades occurred. Typically, the magnitude of the blockades was large (the current was reduced by 85–100%) and, depending on polymer length, the blockades lasted from several hundred to several thousand microseconds. For a given polymer size, the total number of transient blockades was directly proportional to polymer molar concentration (not shown). Virtually no blockades were observed in the absence of poly[U] (Fig. 1) or if the potential across the bilayer was reversed (not shown). Occasionally, after adding polymer, long-lived blockades of several seconds or more occurred which could be cleared by briefly reducing the voltage to 0, or by reversing the polarity of the potential. We assume that these indefinitely long blockades were produced when a polynucleotide entered but could not completely traverse the channel because of entangling secondary structure. The millisecond time scale blockades were also seen in similar experiments with poly[A], poly[C], poly[dT], poly[dC], as well as with single-stranded synthetic DNA composed of 150 nt of poly[dA, dT, dC] (see Materials and Methods).

If the blockades were caused by the transport of extended linear polynucleotides through the channel, the blockade lifetimes should be proportional to the length of the polymer and inversely proportional to the applied potential. A histogram of the current blockade lifetimes for 210-nt-long poly[U] shows that the blockades cluster into three distinct peaks (Fig. 2). Similar histograms for other size selected poly[U]s demonstrated that the mean lifetimes for peaks 2 and 3 were related to polymer length and inversely related to the applied potential (Fig. 3). On the other hand, the numerous fast blockades in peak 1 were independent of polymer length (Fig. 3ω) or applied potential. We attribute these fast peak 1 blockades to polymers that collided with the channel, or partially entered but failed to traverse the channel. Thus, only the blockades in peaks 2 and 3, whose lifetimes were proportional to polymer length, appeared to be the result of polymers that traversed the channel.

Although the length dependency for peaks 2 and 3 was consistent with the notion that a polynucleotide traversed the channel as an extended linear chain, we were surprised that passage through the channel of relatively monodisperse, unbranched polymers would produce blockades whose lifetimes fell under two distinct peaks that contained approximately equal numbers of events. An explanation for the presence of these two peaks is that the characteristic times for polymer transit in the 3′ to 5′ direction may differ from that in the 5′ to 3′ direction. If true, the physical basis for such a difference remains to be explained.

The 2.6-nm diameter of the α-hemolysin channel is apparently too narrow to allow passage of double-stranded polynucleotides because blunt-ended double-stranded DNA produced only the rapid blockades similar to peak 1 events. We also tested mixtures containing equal concentrations of diverse length poly[A] with poly[U] or diverse length poly[dC] with poly[dG]. Such preparations would contain many base paired regions surrounded by unpaired single-stranded ends that might enter the channels but stop at a region of paired bases. As expected, these preparations produced indefinitely long blockades that required voltage polarity reversal to be cleared.

To demonstrate that blockades were attributable to DNA traversing the channels, we performed experiments to compare the number of blockades observed in peaks 2 and 3 with the number of single-stranded molecules that actually tra-

![Fig. 1. Oligomers of poly[U] caused transient blockades in the α-hemolysin single channel current. At the first arrow, a potential of −120 mV was applied across the membrane (cis side negative). This voltage caused a continuous current of −120 pA to flow. At the second arrow, poly[U] of mean length 210 bases was stirred into the cis compartment to a final concentration of 0.1 mg/ml. The polynucleotides caused short-lived current blockades. The inset (expanded time scale) shows two typical blockades with lifetimes of 300 and 1300 μs. For the purposes of illustration, the low time resolution current recordings (a total of 4 sec is shown here) were digitally filtered using an exponential smoothing moving average algorithm.](https://example.com/image1)

![Fig. 2. The characteristic lifetimes of channel blockades caused by poly[U] (0.1 mg/ml; mean length, 210 nt) fell within three well-defined peaks. The mean lifetimes corresponding to the three peaks were determined by fitting the sum of three Gaussians to the data.](https://example.com/image2)
The discovery that a polynucleotide can easily be drawn through a single, well-defined channel provides a simple system for measuring the driven motion of polymers through constraints, a basic problem underpinning many biological processes, as well as gel electrophoresis (27). Recent theories of polymer translocation through a single membrane pore (28) and through multipore (22) could easily be tested in this system.
Fig. 5. Enzymatic hydrolysis of poly[U] caused a transient increase in the rate of oligonucleotide-induced channel blockades. In two separate experiments, at time 0, ribonuclease A (bovine pancreatic RNase Type XII-A; Sigma or Worthington) was added to the cis chamber containing either 0.13 mg/ml poly[U] (●) (mean length, 1100 nt) or 0.27 mg/ml poly[A] (○) (mean length, 20,000 nt; Fluka). The final ribonuclease concentrations were 0.04 mg/ml (poly[U] experiment) or 0.13 mg/ml (poly[A] experiment). Blockade rates were calculated from single channel recordings. The Inset shows ½-sec sample traces for the poly[U] experiment before (Upper) and ~30 sec after (Lower) addition of ribonuclease. Similar experiments with a poly[U] sample of greater length (3000 nt) yielded results comparable to those obtained with the 1100-nt poly[U]. The current was digitized using a SONY/Dagan DAT recorder at 48,000 points/sec.

The realization that single channel measurements can be used to determine the lengths of individual RNA or DNA chains suggests that other characteristics of a polynucleotide could also be measured as the molecule traverses the channel. In principle, a single purine or pyrimidine nucleotide passing through the limiting aperture of a channel should block the ionic current in a manner that reflects the molecular size and chemical properties of each nucleotide in a polynucleotide. If so, it may be possible to use single channel recordings to directly determine the sequence of a polynucleotide. For this to be possible, at least five conditions must be met: each nucleotide must produce a characteristic transient current blockage, the limiting aperture of the channel must have appropriate dimensions to reflect the presence of only one nucleotide at a time, the time resolution of ionic flow measurement must exceed the rate of nucleotide movement through the channel, backward movement of the polynucleotide must be minimal, and the channel and membrane must be sufficiently robust to withstand whatever temperature and chemical treatments are required to eliminate interference from polynucleotide secondary structure.

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