The Cortical Signature of Alzheimer's Disease: Regionally Specific Cortical Thinning Relates to Symptom Severity in Very Mild to Mild AD Dementia and is Detectable in Asymptomatic Amyloid-Positive Individuals

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Alzheimer’s disease (AD) is associated with neurodegeneration in vulnerable limbic and heteromodal regions of the cerebral cortex, detectable in vivo using magnetic resonance imaging. It is not clear whether abnormalities of cortical anatomy in AD can be reliably measured across different subject samples, how closely they track symptoms, and whether they are detectable prior to symptoms. An exploratory map of cortical thinning in mild AD was used to define regions of interest that were applied in a hypothesis-driven fashion to other subject samples. Results demonstrate a reliably quantifiable in vivo signature of abnormal cortical anatomy in AD, which parallels known regional vulnerability to AD neuropathology. Thinning in vulnerable cortical regions relates to symptom severity even in the earliest stages of clinical symptoms. Furthermore, subtle thinning is present in asymptomatic older controls with brain amyloid binding as detected with amyloid imaging. The reliability and clinical validity of AD-related cortical thinning suggests potential utility as an imaging biomarker. This “disease signature” approach to cortical morphometry, in which disease effects are mapped across the cortical mantle and then used to define ROIs for hypothesis-driven analyses, may provide a powerful methodological framework for studies of neuropsychiatric diseases.

Keywords: Alzheimer’s disease, cerebral cortex, magnetic resonance imaging, medial temporal lobe, parietal cortex

Introduction

The symptoms of Alzheimer’s disease (AD)—progressive impairment in memory, executive function, visuospatial abilities, language, and behavior—arise from neurodegeneration of specific brain regions, prominently including the paralimbic and heteromodal association areas. Initially, knowledge of brain regions selectively vulnerable to AD was obtained from post-mortem brain tissue (Brun and Gustafson 1976; Arnold et al. 1991; Braak and Braak 1991; Morrison and Hof 2002). In the past 15 years, magnetic resonance imaging (MRI) has provided insights into quantitative neuroanatomic abnormalities in living individuals with AD as well as the progressive course of the disease. Volume loss in specific regions, such as the hippocampal formation (Jack et al. 1992; Killiany et al. 1993) and entorhinal cortex (Juottonen et al. 1998; Bobinski et al. 1999; Killiany et al. 2000; Dickerson et al. 2001), can be detected in vivo using manual region-of-interest MRI techniques. Manual methods are labor-intensive and typically focus on a few a priori-defined regions, which has resulted in the extensive study of some regions of the brain that are well known to be affected by AD (e.g., the hippocampal formation and entorhinal cortex) without equivalent study of the distributed network of all brain regions affected. Analysis of differences in whole-brain volume between individuals with early AD and controls (Fotenos et al. 2005) as well as accelerated whole-brain atrophy rates in AD (Fox et al. 1999; Cardenas et al. 2003; Fotenos et al. 2005) make clear that extensive regional changes are taking place in AD because changes localized to the medial temporal lobe simply cannot account for such large-scale effects, which are present even at the earliest stages of the disease. As an extreme example, clinically nondemented individuals (Clinical Dementia Rating [CDR] = 0) with positive amyloid binding as measured using positron emission tomography (PET) show reduced whole-brain volumes relative to amyloid-free peers suggesting that cortical atrophy may be present before clinical symptoms appear (Fotenos et al. 2008).

These observations raise several questions that can be investigated using MRI measures. First, of the spatially distributed cortical regions that are most prominently affected in AD, does the relative magnitude of atrophy suggest a sequence of involvement similar to that hypothesized from post-mortem studies? Is the pattern of vulnerable cortical regions consistent from one group of individuals with AD to the next? And how early in the progression of the disease can differences in vulnerable cortex be detected? The answers to these questions will provide in vivo data about the brain networks affected in AD that can complement neuropathological data as well as identify affected cortical regions for use as biomarkers for detection and monitoring of AD.
Insights into the distributed cortical regions that show atrophy in AD have begun to emerge. Computational MRI data analysis methods based on voxel-based morphometry or analysis of local cortical deformations provide maps of estimated gray matter atrophy in AD without a priori focus on specific regions (Baron et al. 2001; Thompson et al. 2001; Frisoni et al. 2002; Good et al. 2002; Scalfi et al. 2002; Karas et al. 2003; Buckner et al. 2005). Consistent with expectations, these studies reveal effects of AD on distributed regions of cortex including posterior lateral temporoparietal and medial parietal regions as well as robust effects in medial and lateral temporal cortex. Methods have also been developed that enable the measurement of cortical thickness across the entire cortical mantle (Fischl and Dale 2000; MacDonald et al. 2000; Kabani et al. 2001; Rosas et al. 2002). Initial studies of cortical thickness demonstrate thinning in distributed association areas again suggesting that regional atrophy can be detected across widespread cortical regions (Lerch et al. 2005; Du et al. 2007). One advantage of the measurement of cortical thickness is that it provides a quantitative value that represents a physical property of the brain that can be measured in an individual person, whether in vivo or from post-mortem tissue (Rosas et al. 2002).

Here we expanded upon prior work on cortical thinning in AD in several important ways. First, although voxel-based studies have included patients with milder forms of AD (Karas et al. 2004; Rozzali et al. 2006; Apostolova et al. 2007; Whitwell et al. 2008), previous studies of cortical thinning in AD have included patients with dementia severity ranging from mild to moderate AD, so the relative magnitude and pattern of cortical thinning in the mildest clinical phases of AD is unclear. In the present study we focused specifically on AD at mild and very mild stages of the disease. Moreover, there has been little investigation of the relationship between cortical thinning and severity of symptoms in patients with the mildest symptoms of AD. We explored this relationship directly. Second, we examined AD-associated cortical thinning across 4 independent samples from multiple sites and scanners. This allowed us to investigate the consistency of cortical thinning across multiple data samples and also, by pooling the data across sites, provide a highly precise large-sample estimate of the regional magnitude of cortical thinning in AD. By comparing data across sites this study also provides evidence for the feasibility of such analyses for multicenter clinical studies (e.g., the Alzheimer’s Disease Neuroimaging Initiative [Mueller et al. 2005]).

Recent in vivo data using the amyloid-imaging tracer \[^{11}C\]Pittsburgh Compound B (PIB) (Klunk et al. 2004) indicate that some clinically normal (asymptomatic) older individuals harbor fibrillar amyloid deposits, consistent with a presymptomatic AD state (Buckner et al. 2005; Mintun et al. 2006). Although previous data suggest that regional deposition of amyloid overlaps in part with areas of cortical atrophy in AD (Buckner et al. 2005), the question of whether it is possible to detect subtle regional cortical thinning in older individuals with brain amyloid has never been investigated. Based on previous work in which atrophy was detected in asymptomatic individuals prior to their conversion to very mild dementia (Buckner et al. 2005), we hypothesized that it may be possible, by focusing on the regions known to be affected in clinically mild AD, to detect a subtle degree of cortical thinning in amyloid-positive asymptomatic individuals.

**Participants and Methods**

**Overview**

Analyses proceeded in several steps that involved data from 380 participants (336 using structural MRI and 44 using amyloid-PIB PET and structural MRI). First, in a large primary sample of participants (N = 144), we explored the entire cortical mantle to identify areas of thinning in a relatively homogeneous sample of participants with mild AD (N = 29) compared with nondemented older controls (OC, N = 115). This initial analysis identified a cortical signature of AD—a spatially distributed set of specific regions with AD-related thinning. Regions of interest (ROIs) were defined to capture the spatially distributed pattern of cortex most affected by AD. Then, to investigate the consistency of cortical thinning in AD, we applied these a priori ROIs to 3 new samples of AD participants and OC (total N = 123). Each independent sample was recruited and evaluated at a different clinical site and scanners involved 2 different field strengths (1.5 and 3 T), similar to multicenter studies such as clinical trials. To explore the progression of AD, we next applied the a priori ROIs to another sample of individuals with Incipient and very mild AD dementia (N = 69) to determine the degree to which these regions are affected in the earliest clinical stages of disease progression. The relationship of regional cortical thinning to severity of symptoms was also investigated by correlational analysis between ROI thickness and the Clinical Dementia Rating scale Sum-of-Boxes (Morris et al. 1997), a measure of severity of cognitive and functional impairments in daily life. A pooled analysis was performed of all 267 mild AD patients and OC to provide a stable, highly precise estimate of the spatial distribution and magnitude of thinning in the cortical signature of AD. Finally, “AD-signature” regional thickness was investigated in a group of OC individuals known to harbor brain amyloid from PIB-PET scanning and compared with a group of OC individuals without brain amyloid.

The overall data collection and analysis procedure is depicted in a flowchart in Figure 1. Demographic and clinical data for the participants are presented in Table 1.

**Sample 1a**

The primary sample included a total of 144 participants (Sample 1a; see Table 1 for demographic and clinical data). Data from subsets of the participants have been published in previous studies (Buckner et al. 2004, 2005; Salat et al. 2004; Fotenes et al. 2005).

All participants in this sample were recruited from the ongoing longitudinal study of the Washington University AD Research Center (ADRC) using procedures approved by Washington University’s human subjects committee. At study enrollment, participants were clinically free of non-AD disorders that could potentially cause dementia such as major depression, stroke, Parkinson disease, and head trauma (Berg et al. 1998).

Trained clinicians assessed each participant for the presence and severity of dementia based on semi-structured interviews with the participant and a knowledgeable informant (usually a spouse or adult child) followed by a neurological examination of the participant (Morris 1993; Morris et al. 1997). Also included in the protocol are a health history, depression inventory, aphasia battery, and medication inventory. The CDR staging and clinical diagnostic determinations were made by the examining clinician. Diagnostic criteria for AD required the gradual onset and progression of impairment in memory and in at least one other cognitive and functional domain, comparable to standard diagnostic criteria for probable AD (McKhann et al. 1984).

For the purposes of the present study, the resultant clinical diagnostic categories include normal OC (CDR = 0, Mini Mental State Examination [MMSE] 25–30, N = 115) or mild dementia of the Alzheimer type (referred to here as AD; CDR = 1, MMSE 15–28, N = 29). In addition, we studied another sample of subjects recruited and evaluated in the same manner who exhibited a milder level of impairment (Sample 1b). Within the CDR = 0.5 category, the 2 diagnostic groups are distinguished based on the clinical judgment of the evaluating clinician with respect to the degree to which symptoms of cognitive impairment impact the individual’s independent function in daily life, as described previously: very mild AD (CDR = 0.5, MMSE 14–30, N = 40) or incipient AD (CDR = 0.5, MMSE 24–30, N = 29) (Morris et al. 2009).
et al. 1988, 2001; Morris 1993; Berg et al. 1998; Storandt et al. 2006). Many of these CDR = 0.5 individuals would be classified as having mild cognitive impairment in other settings (Morris et al. 2001; Storandt et al. 2006).

An additional 44 participants were asymptomatic normal OC (CDR = 0, MMSE 26-30) and had both amyloid-PiB PET data available (see below) as well as MRI data—this was Sample 1c.

Multiple (3 or 4) high-resolution structural T1-weighted magnetization-prepared rapid gradient echo (MP-RAGE) images were acquired on a 1.5T Siemens Vision scanner (Siemens Medical Systems, Erlingan, Germany) with the following parameters: repetition time (TR) 9.7 ms, echo time (TE) 4 ms, flip angle (FA) 10, inversion time (TI) 20 ms, voxel size 1 x 1 x 1.25 mm. These data have been made openly available to the community (http://www.oasis-brains.org/).

### Table 1

Demographic and clinical characteristics of participants

<table>
<thead>
<tr>
<th>Sample Group</th>
<th>N</th>
<th>Age (M/F)</th>
<th>MMSE</th>
<th>CDR Sum-of-boxes</th>
</tr>
</thead>
<tbody>
<tr>
<td>1a OC</td>
<td>115</td>
<td>77.2 ± 8.4</td>
<td>29.1 ± 1.1</td>
<td>0 ± 0</td>
</tr>
<tr>
<td>1b Mild AD</td>
<td>29</td>
<td>77.5 ± 6.5</td>
<td>22.1 ± 3.5*</td>
<td>0/0/9</td>
</tr>
<tr>
<td>1c Very mild AD</td>
<td>40</td>
<td>76.0 ± 6.3</td>
<td>25.2 ± 3.8*</td>
<td>0/40/0</td>
</tr>
<tr>
<td>2 OC</td>
<td>29</td>
<td>78.1 ± 7.1</td>
<td>29.3 ± 0.6</td>
<td>0 ± 0</td>
</tr>
<tr>
<td>2b OC</td>
<td>22</td>
<td>78.1 ± 2.2</td>
<td>29.3 ± 0.8*</td>
<td>0/0/9</td>
</tr>
<tr>
<td>3 OC</td>
<td>29</td>
<td>78.1 ± 3.7</td>
<td>29.4 ± 0.9</td>
<td>28/0/0</td>
</tr>
<tr>
<td>3b Mild AD</td>
<td>17</td>
<td>81.9 ± 6.6</td>
<td>24.6 ± 2.8*</td>
<td>0/0/9</td>
</tr>
<tr>
<td>4 OC</td>
<td>15</td>
<td>78.3 ± 6.2</td>
<td>29.6 ± 0.5</td>
<td>0 ± 0</td>
</tr>
</tbody>
</table>

Note: Values represent mean ± standard deviation. *P < 0.001 (different from OC). BDS-IMC = Blessed Dementia Score Information-memory-concentration.

MMSE scores calculated from Blessed IMC scores (Thal et al. 1986).

### Additional Participant Samples

Data from 3 additional samples of nondemented OC participants and AD patients were analyzed as part of this study. The 3 samples were drawn from separate ongoing studies at Massachusetts General Hospital, all of which were approved and conducted in accordance with guidelines established by the Partners Human Research Committee. Written informed consent was obtained from each participant, and from a caregiver for patients with AD with significant cognitive impairment. See Table 1 for detailed demographic and clinical data on these additional samples.

Assessments were conducted in a manner nearly identical to that described above (details have been previously published as cited below), with 39 participants in Sample 2 (Atri et al. 2005), 41 participants in Sample 3 (Wright, Dickerson, et al. 2007; Wright, Feczko, et al. 2007), and 40 participants in Sample 4 (Dickerson et al. 2005; Celone et al. 2006). The characteristics of the AD dementia participants in these samples were as follows; see also Table 1. In Sample 2, AD dementia participants had CDR = 0.5 (N = 10) or CDR = 1 (N = 7); mean MMSE = 21.5 (SD = 3.9), range 12-29. In Sample 3, AD participants had…

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**Figure 1.** Flowchart of methodologic procedures employed in this study and specific analyses used to generate figures (Fig) and tables (Tbl). Shaded rows at bottom show the specific subject samples (S) that were used to generate each table and figure. For example, Samples 1a and 1b were used to generate Figure 4 and Table 4 (second shaded row). See Table 1 for details of diagnostic groups and demographic and clinical characteristics of each sample.
CDR = 0.5 (N = 2) or CDR = 1 (N = 10); mean MMSE = 24.6 (SD = 2.8), range 20–29. In Sample 4, AD participants had CDR = 1; mean MMSE = 23.3 (SD = 4.2), range 15–30.

Samples 2 and 3 were scanned in an identical manner on 2 different Siemens 1.5T scanners (Sample 2 on an Avanto with 12 channel Total Imaging Matrix head coil and Sample 3 on a Sonata with 3-axis gradient single channel head coil; Siemens Medical Systems, Erlingan, Germany). For both samples, 2 high-resolution structural T1-weighted MP-RAGE images were acquired with the following parameters: TR 2730 ms, TE 3.31 ms, FA 7, TI 1000 ms, voxel size 1.5 × 1 × 1 mm. Sample 4 was scanned as follows: one high-resolution structural T1-weighted MP-RAGE image was acquired on a 3.0T Siemens Trio scanner (Siemens Medical Systems, Erlingan, Germany) with a 3-axis gradient head coil with the following parameters: TR 2530 ms, TE 3.45 ms, FA 7, TI 1100 ms, voxel size 1.3 × 1 × 1 mm. For all samples, procedures for data collection included head movement restriction using expandable foam cushions, and automated scout and shimming procedures.

**Estimation of Cortical Thickness**

Methods for our surface-based analyses and estimation of cortical thickness have been previously described in detail (Dale et al. 1999; Fischl, Sereno, and Dale 1999; Fischl and Dale 2000; Rosas et al. 2002; Kuperberg et al. 2003; Salat et al. 2004) and are described here only briefly. The FreeSurfer software used to perform the analyses and visualization employed in this study, along with complete documentation, is freely available via the internet at http://surfer.nmr.mgh.harvard.edu.

First, the multiple MP-RAGE acquisitions for each participant were motion corrected and averaged to create a single image volume with high contrast-to-noise (sample #4 involved a single acquisition, so this was used for subsequent processing). The resulting averaged volume was used to segment cerebral white matter (Dale et al. 1999) and to estimate the location of the gray/white boundary. Topological defects in the gray/white boundary were corrected (Fischl et al. 2001), and this gray/white boundary was used as the starting point for a deformable surface algorithm designed to find the pial surface with submillimeter precision (Fischl and Dale 2000). Cortical thickness measurements were obtained by calculating the distance between those surfaces at each of approximately 160,000 points (per hemisphere) across the cortical mantle (Fischl and Dale 2000). The thickness measures derived from this technique are both valid (Rosas et al. 2002; Kuperberg et al. 2003) and reliable (Han et al. 2006; Dickerson et al. 2008).

The surface representing the gray-white border was “inflated” (Fischl, Sereno, and Dale 1999), differences among individuals in the depth of gyri and sulci were normalized, and each subject’s reconstructed brain was then morphed and registered to an average spherical surface representation that optimally aligns sulcal and gyral features across participants (Fischl, Sereno, and Dale 1999; Fischl, Sereno, Tootell, et al. 1999). Thickness measures were then mapped to the inflated surface of each participant’s reconstructed brain (Fischl, Sereno, and Dale 1999). The data were smoothed on the surface using an iterative nearest-neighbor averaging procedure. One hundred iterations were applied, which is equivalent to applying a 2-dimensional Gaussian smoothing kernel along the cortical surface with a full-width/half-maximum of 18.4 mm. Data were then resampled for participants into a common spherical coordinate system (Fischl, Sereno, Tootell, et al. 1999).

**Hypothesis-Driven Statistical Analysis of Additional Samples**

We next investigated the magnitude of AD-related thinning within cortical regions identified in the exploratory analysis in 3 independent data samples. For regions in which there was a statistical effect in Sample 1a, an ROI label was drawn on the average cortical surface template. These ROI boundaries followed the “AD effects” identified through the exploratory analysis, not gyral or sulcal anatomical boundaries. Figure 2 shows the statistical AD effects from the exploratory analysis, and the map in Figure 3 shows ROIs derived from this analysis. Nine AD-signature ROIs were drawn in each hemisphere; the effects were relatively symmetric and the differences were present the basic size and shape characteristics of ROIs were kept similar across hemispheres. In addition to the 9 AD-effect ROIs, a “primary visual cortex” ROI label was drawn in the calcarine fissure to serve as a control ROI. Using the spherical registration of each subject to the template, the 10 cortical ROIs (per hemisphere) were mapped back to individual participants. For each subject, mean cortical thickness within each ROI was calculated by deriving an average of all of the thickness estimates at vertices that fell within the labeled ROI.

For each subject, the resultant ROI measures of cortical thickness were averaged across the 2 hemispheres, and these 10 values per subject were used for further statistical analysis. These ROI thickness values were used to calculate the mean difference in the thickness of each ROI between the AD and OC groups, the percent thinning in AD in relation to OC, and the Cohen’s $d$ effect sizes of AD-related thinning for each ROI. Group comparisons were performed using analyses of variance (ANOVAs), with a priori specified planned contrasts, to evaluate differences between the AD and OC groups within each sample. Analyses were repeated with age and sex as covariates to ensure that there were no significant influences of these variables. Cortical thickness is not correlated with head size (data not shown), so is not adjusted (i.e.,...
for intracranial volume). There were no hemispheric effects in these analyses, so measures from both hemispheres were pooled to make one measure of mean cortical thickness for each subject. Pearson correlations and a multiple linear regression analysis was performed to examine relationships between thickness of the 10 cortical ROIs and the measure of AD severity (the CDR Sum-of-Boxes; Morris et al. 1997). These statistical analyses were performed using SPSS 11.0 (SPSS, Chicago, IL). All analyses were performed with a statistical threshold for significance of $P < 0.05$, uncorrected for multiple comparisons.

**[11C]PIB PET Maps of Amyloid Deposition**

We used [11C]PIB (Klunk et al. 2004) to image amyloid in a sample of nondemented OC individuals (Sample 1c). Participants were imaged using [11C]PIB on a 961 ECAT PET scanner (Siemens, Erlangen, Germany) according to the procedures described previously (Buckner et al. 2005; Mintun et al. 2006). PIB-PET imaging provides an in vivo measure of human brain amyloid in plaques associated with AD (Klunk et al. 2004; Buckner et al. 2005; Mintun et al. 2006). Individuals were considered PIB negative if their binding potential for 4 cortical regions (prefrontal, lateral temporal, precuneus, and gyrus rectus) was below 0.2 (Fagan et al. 2006; Mintun et al. 2006; Fotenos et al. 2008). For the purposes of the present study, we used PIB-PET imaging to identify a subset of 9 older individuals who were cognitively intact but harbored significant amyloid deposition. The present classification of participants is the same as that used by a previous study (Fotenos et al. 2008) of whole-brain atrophy.

**Results**

**Analysis of Mean Cortical Thickness**

In Sample 1a, this analysis revealed an effect of AD, with the mild AD group showing 4.5% mean cortical thinning compared with OC (OC = 2.14 [SD = 0.08] mm, AD = 2.05 [0.11] mm; $F(1) = 26.2, P < 0.001$, Cohen’s $d = 1.02$). Across the other 3 samples of participants, very similar effects were found. In Sample 2, mean cortical thickness of the AD group was 5.5% thinner than controls (OC = 2.03 [0.10] mm, AD = 1.92 [0.13] mm; $F = 11.2, P < 0.002$, Cohen’s $d = 1.0$). In Sample 3, the AD group’s mean cortical thickness was 6.5% thinner than controls (OC = 2.13 [0.09] mm, AD = 2.00 [0.11] mm; $F = 19.5, P < 0.001$, Cohen’s $d = 1.41$). Finally, in Sample 4, scanned at 3.0 Tesla, mean cortical thickness of the AD group was 6.0% thinner than controls (OC = 2.16 [0.09] mm, AD = 2.03 [0.10] mm; $F = 17.1, P < 0.001$, Cohen’s $d = 1.34$).

Similar analyses were also performed to investigate these measures in the 2 subject groups with milder levels of impairment (CDR = 0.5, Sample 1b). The group with very mild AD showed effects similar to, but of a lesser magnitude than, those of the mild AD group: 3.7% mean cortical thinning compared with controls (very mild AD = 2.06 [0.10] mm; $F = 23.6, P < 0.001$, Cohen’s $d = 0.87$). The group with incipient AD showed no reduction in mean cortical thickness compared with controls (mean cortical thickness = 2.12 [0.11] mm; $P = 0.32$).

**Regionally Specific Cortical Thinning in Mild AD: Exploratory Analysis across the Entire Cortical Mantle**

In Sample 1a, the exploratory analysis of cortical thickness across the entire mantle revealed a set of specific regions that...
were thinner in AD than OC, as illustrated in Figure 2. Regions of significant thinning were primarily located in limbic and heteromodal association areas, including rostral medial temporal, inferior temporal, temporal pole, precuneus, inferior parietal (supramarginal and angular gyri), superior parietal, inferior frontal, and superior frontal cortex. There were minor differences in the spatial location of regional thinning across hemispheres, but generally the regions were quite consistent bilaterally. Primary sensorimotor regions were largely spared.

**Quantitative Analysis of Cortical Regions Vulnerable to AD**

We next investigated the magnitude of AD-related thinning within each cortical region identified in the exploratory analysis. Cortical ROI label locations and group mean and standard error data are shown in Figure 3. Data for Sample 1a is shown in the leftmost pair of bars in each graph in Figure 3. Mean thickness, standard deviation, magnitude of group differences (in mm), percent thinning in AD compared with controls, and Cohen’s d effect sizes are shown in Table 2.

Thinning due to AD was most prominent (in mm) in the rostral medial temporal cortex, with a mean magnitude of thinning of more than 0.4 mm (14% thinning in AD compared with OC). Other regions with more than 0.2 mm thinning included inferior temporal, temporal pole, inferior parietal (both angular and supramarginal gyri), and superior frontal regions, which ranged from 8.1% to 11.6% thinner in AD than OC. The regions with a relatively smaller magnitude of thinning (0.16–0.19 mm, or 7–8%) included precuneus, inferior frontal, and superior parietal regions. There was no significant thinning in the primary visual cortex (0.03 mm [2.2%], \( P = 0.19 \)).

**Consistency of Regional Cortical Thinning in Mild AD: Quantitative Analysis of Cortical Regions in 3 Separate Samples**

The consistency of regionally specific cortical thinning was investigated in 3 additional samples of AD patients and OC individuals. This analysis was unbiased, as it employed cortical ROIs defined as above from Sample 1a and applied to separate samples of participants (by mapping each cortical ROI label from the average surface template to each individual via the spherical average surface, as described in Methods).

The magnitude of AD-related thinning within these cortical regions was remarkably consistent across the 3 additional samples. Figure 3 illustrates the mean thickness and standard error with regions across all 4 samples. Table 3 provides details of measurements from Samples 2, 3, and 4, showing magnitude of group difference (AD vs. OC), percent thinning in AD, and effect sizes.

Again, across all 3 additional samples, the medial temporal cortex showed the largest magnitude of thinning of all regions within each sample, ranging from 0.26 to 0.55 mm thinner in AD than OC. Temporal pole and inferior parietal regions showed consistently large effects, whereas inferior temporal, superior parietal, precuneus, and frontal regions were somewhat less consistent with respect to magnitude of thinning. Primary visual cortex again showed no effects in these 3 samples.

An additional analysis was performed to investigate thickness differences between the 4 samples. A main effect was found for Sample 2, with mean cortical thickness biased toward slightly thinner estimates without an interaction with diagnostic group.

**Detection of Attenuated Regional Cortical Thinning in Individuals with Milder Symptoms of AD**

We next investigated a sample (Sample 1b) of individuals with milder symptoms of AD to determine whether a lesser magnitude of cortical thinning would be detectable within regions known to be vulnerable to AD from the analyses above. All of these participants had an overall CDR rating of 0.5, but some were diagnosed with very mild AD (\( n = 40 \)) and others were diagnosed with incipient AD (\( n = 29 \)). See Table 1 for demographic and clinical data on these participants. The AD-signature cortical ROI labels, as defined from Sample 1a, were again applied to this sample of individuals with very mild AD or incipient AD.

AD-related thinning was detected within these cortical regions in a remarkably consistent manner across the 2 milder groups. Most of the regions demonstrated a pattern suggestive of progressive thinning across the 4 groups, as illustrated in Figure 4. The primary visual cortex showed no such effect. As depicted in Table 4, statistical analysis demonstrated that the all regions except the primary visual cortex were thinner in the very mild AD group than OC. Inspection of the percent thinning in very mild AD reveals a lesser degree of thinning in all regions than in the mild AD group. The magnitude of thinning in the incipient AD group is relatively small in all regions, with most differences in regional thickness compared with OC not reaching statistical significance (except angular and supramarginal gyri). The primary visual cortex ROI shows...
Table 4
Quantitative metrics of thinning by region within incipient and very mild AD participants

<table>
<thead>
<tr>
<th>Region</th>
<th>Mean thickness (mm) (SD)</th>
<th>Percent thinning (vs. OC)</th>
<th>Effect Size (vs. OC)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>OC</td>
<td>Incipient AD</td>
<td>Very mild AD</td>
</tr>
<tr>
<td>Medial temporal</td>
<td>2.91 (0.33)</td>
<td>2.90 (0.30)</td>
<td>2.63 (0.37)</td>
</tr>
<tr>
<td>Temporal pole</td>
<td>2.67 (0.23)</td>
<td>2.62 (0.23)</td>
<td>2.53 (0.20)</td>
</tr>
<tr>
<td>Angular</td>
<td>2.32 (0.16)</td>
<td>2.21 (0.18)</td>
<td>2.16 (0.14)</td>
</tr>
<tr>
<td>Superior frontal</td>
<td>2.55 (0.17)</td>
<td>2.49 (0.20)</td>
<td>2.43 (0.19)</td>
</tr>
<tr>
<td>Superior parietal</td>
<td>2.02 (0.13)</td>
<td>1.98 (0.18)</td>
<td>1.92 (0.13)</td>
</tr>
<tr>
<td>Supramarginal</td>
<td>2.38 (0.17)</td>
<td>2.28 (0.16)</td>
<td>2.26 (0.18)</td>
</tr>
<tr>
<td>Precuneus</td>
<td>2.21 (0.18)</td>
<td>2.15 (0.28)</td>
<td>2.08 (0.22)</td>
</tr>
<tr>
<td>Inferior frontal</td>
<td>2.16 (0.13)</td>
<td>2.14 (0.14)</td>
<td>2.03 (0.19)</td>
</tr>
<tr>
<td>Primary visual</td>
<td>1.51 (0.12)</td>
<td>1.52 (0.16)</td>
<td>1.50 (0.12)</td>
</tr>
</tbody>
</table>

Note: Superscripts indicate that the group is significantly different from OC (C), incipient AD (I), very mild AD (V), or mild AD (A) (\(P < 0.05\), uncorrected). Percent thinning is in comparison to OC group (data presented in Table 3). Effect size is Cohen’s \(d\).

a remarkable degree of reliability with respect to absolute cortical thickness across the groups (lower right graph in Fig. 4). Figure 4 illustrates the mean thickness and standard error within regions across the very mild AD and incipient AD groups, with the OC and mild AD groups shown for comparison. Table 4 provides details of measurements from these 2 groups of participants.

**Relationship of Regional Cortical Thinning to Severity of Clinical Impairment**

We analyzed the relationship of the regional measures of cortical thickness to severity of symptoms of cognitive impairment within all the demented participants from Washington University (incipient AD, very mild AD, mild AD; \(N = 97\)). Correlational analyses were run with the CDR Sum-of-Boxes (CDR-SB) as the dependent measure. Although the overall CDR ratings (0.5 or 1) of these individuals indicated that they were very mildly or mildly demented, the CDR-SB provides a finer grading of impairment within this spectrum, ranging in this sample of mildly demented, the CDR-SB provides a finer grading of clinical impairment within this spectrum, ranging in this sample of mild AD.

These correlative analyses with CDR-SB were also examined within the diagnostic groups. The mild AD group demonstrated trends for superior (\(R = -0.35, P = 0.06\)) and inferior frontal (\(R = -0.32, P = 0.08\)) regions, whereas the very mild AD group demonstrated an effect for the medial temporal cortex (\(R = -0.34, P = 0.03\)) and a trend for the angular gyrus (\(R = -0.28, P = 0.08\)). There were no effects in the incipient AD group.

**Pooled Multicenter Mapping Analysis of the Magnitude of Cortical Thinning in Mild AD**

For this analysis, a general linear model was constructed that included all 4 mild AD and all 4 OC groups. Each participant contributed a cortical thickness estimate mapped to the group using spherical registration. The contrast of interest was AD versus OC, and was weighted according to the number of participants in each group. The parameter estimate of difference in cortical thickness between AD and OC was then used to generate a map of the magnitude of cortical thinning in AD. Note that this map is quantitative revealing the estimated size (in mm) of cortical thinning. Thus, this map reflects our best estimate of the topography and magnitude of cortical thinning in mild AD.

Figure 5 illustrates the results of the pooled analysis, which was undertaken to map the magnitude of thinning across the entire cerebral cortex in Samples 1a, 2, 3, and 4 comparing AD with OC (total \(N = 267\)). Areas of the cortex in which the magnitude of AD-related thinning exceeds 0.15 mm are shown, using a color scale to indicate the magnitude of thinning. The spatial topography of regional thinning parallels that illustrated with the statistical map of Sample 1a alone (Fig. 2). The areas with the greatest magnitude of thinning across this large multicenter dataset, such as medial temporal cortex, are quite similar to those indicated by the ROI analyses of thinning within each sample above. The congruence of the effects detected with this pooled analysis and those detected above using hypothesis-driven replication samples supports the feasibility of pooled analyses of cortical thickness in multisite/multiscanner data using the high-throughput computational analysis system. A Supplementary Table provides the estimates of the magnitude of thinning in AD for the entire pooled sample.

**Detection of Regional Cortical Thinning in Amyloid-Positive Asymptomatic Older Individuals**

We next investigated a sample (Sample 1c) of individuals evaluated in the same fashion as that described above for Sample 1a, and who were considered to be asymptomatic OC (CDR = 0). Based on PIB-PET scans, they were dichotomized into OC participants with (amyloid-positive, \(N = 9\)) or without (amyloid-negative, \(N = 35\)) PIB amyloid binding. We sought to determine whether subtle cortical thinning might be detectable within regions known to be vulnerable to AD from the analyses above. See Table 1 for demographic and clinical data on these participants. The AD-signature cortical ROI labels, as defined from Sample 1a, were again applied to this sample of amyloid-positive or amyloid-negative OC individuals.
AD-related thinning was detected within the temporal pole (5.8% thinning, \( P = 0.04 \)) and a trend was present in the superior frontal cortex (4.6% thinning, \( P = 0.06 \)) in the amyloid-positive OC group compared with the amyloid-negative OC group. Most other regions demonstrated a pattern suggestive of subtle thinning (see Fig. 7), but the small sample size lacked power for statistical demonstration of effects. Thus, the thickness measures from all 9 ROIs were averaged to create a single mean “AD cortical signature” thickness measure. A trend toward thinning in this mean AD cortical signature measure was present in the amyloid-positive OC group compared with the amyloid-negative OC group (\( P = 0.09 \)). This finding was further supported by a post hoc comparison that demonstrated thinning in the mean AD cortical signature measure of the amyloid-positive OC group compared with the larger OC (amyloid status unknown, \( N = 115 \)) group from Sample 1a (\( P < 0.05 \)). Mean thickness of the entire cortex in the amyloid-positive group (2.17 ± 0.11 mm) did not differ from that of the amyloid-negative group (2.13 ± 0.7 mm) nor from that of the larger OC group from Sample 1a (all \( P \) values > 0.19). Figure 6 illustrates the AD cortical signature measure (mean and standard error of the mean) across the amyloid-positive OC, amyloid-negative OC, and other 4 groups from Samples 1a, 1b, and 1c.

Discussion

The pathology of AD typically has a predilection for limbic allocortical and heteromodal association neocortical areas (Ibrut and Gustafson 1976; Arnold et al. 1991; Braak and Braak 1991). Quantitative analysis of MRI has been used to identify, in living AD patients, abnormalities in the normal anatomic properties—such as volume, gray matter density, and thickness—of the cerebral cortex using manual a priori ROI-based MRI techniques (Jack et al. 1997; Juottonen et al. 1998; Bobinski et al. 1999; Killiany et al. 2000; Dickerson et al. 2001) and more recently using semiautomated exploratory mapping techniques (Baron et al. 2001; Thompson et al. 2001; Good et al. 2002; Scahill et al. 2002; Karas et al. 2003; Buckner et al. 2005; Lerch et al. 2005; Du et al. 2007; Whitwell et al. 2008). In the present work, we pursued a novel approach combining exploratory mapping and a priori ROI-based measurement techniques, first by performing an exploratory analysis of cortical thickness across the entire cortical mantle to map the “cortical signature” of regional thinning in mild AD and then by using this map to generate ROIs to measure, in an a priori fashion, the consistency of regional cortical thinning in multiple independent samples of mild AD patients and the presence of thinning in milder forms of AD.

These additional analyses revealed a lesser magnitude of thinning in patient groups with milder symptoms of AD consistent with mild cognitive impairment (Morris et al. 2001; Storandt et al. 2002, 2006). Even within AD patients spanning the circumscribed spectrum of incipient, very mild, and mild AD, the thickness of many of the critical cortical regions correlates with the relative severity of clinical impairments. Of particular interest, a very mild degree of cortical thinning in these regions was detected in amyloid-positive OC (\( CDR = 0 \)) individuals, indicating that subtle anatomic change in a pattern consistent with AD begins to occur in asymptomatic individuals who harbor AD pathology. To provide a stable estimate of cortical thinning in AD, Figure 5 maps a pooled analysis of the

Figure 4. Thinning in cortical ROIs in incipient and very mild AD participants. ROIs were generated from exploratory analysis in subject Sample 1a (see Fig. 2, same ROIs as used in Fig. 3) and applied to a new sample of Incipient and very mild AD patients (\( CDR = 0.5 \), Sample 1b) to test the hypothesis that these regions are thinner in the mildest clinical stages of AD than controls. Graphs show mean cortical thickness within each ROI across the 2 mildly impaired samples, in comparison to controls and mildly impaired (\( CDR = 1 \)) AD patients (Sample 1a). A primary visual cortex region was also used to illustrate minimal effects on this region (lower right). Error bars indicate 1 standard error of the mean. See Table 3 for statistics. (A) Medial temporal cortex, (B) Inferior temporal gyrus, (C) Temporal pole, (D) Angular gyrus, (E) Superior frontal gyrus, (F) Superior parietal lobule, (G) Supramarginal gyrus, (H) Precuneus, (I) Inferior frontal sulcus, (J) Primary visual cortex.
Figure 5. Magnitude of cortical thinning in AD in millimeters, derived from pooled analysis of 4 samples of participants (Samples 1a, 2, 3, and 4). Map shows parameter estimate of amount of thinning across cerebral cortex from general linear model analysis of 287 participants, showing areas where cortex is at least 0.15 mm thinner in AD group than OC group. Color scale shows magnitude of thinning from 0.15 mm (red) through 0.2 mm (yellow) in AD compared with OC.

Figure 6. Mean thickness of AD cortical signature regions is decreased in amyloid (PiB)-positive OC (CDR = 0), and demonstrates progressive thinning as the symptoms of AD dementia become progressively more prominent across the spectrum of Incipient, very mild, and mild AD dementia. Bars represent mean thickness of the 9 cortical regions shown in Figure 2, normalized for age and standardized to Z scores (y-axis). Error bars indicate 1 standard error of the mean. The leftmost 3 groups are all OC (CDR = 0, MMSE 25–30), ordered by PiB status unknown (unk) (N = 115), PiB negative (N = 35), and PiB positive (N = 9). The rightmost 3 groups are all PiB status unknown, but are progressively more impaired with clinical symptoms ranging from incipient AD (CDR = 0.5/CDR-SB = 1.2, N = 29), very mild AD (CDR = 0.5/CDR-SB = 3.5, N = 40), and mild AD (CDR = 1/CDR-SB = 5.5, N = 29). Figure includes data from Samples 1a, 1b, and 1c.

The magnitude of cortical thinning in all 76 mild AD patients compared with all 194 OC participants from the 4 samples.

Taken collectively, these observations show that this high-throughput, semiautomated MRI data analysis procedure for quantifying cortical thickness is feasible for pooled analysis of multisite data, such as is typical for clinical trials or other large multicenter studies. The method is sensitive enough to detect subtle changes in cortical regions specifically affected by AD prior to the onset of even the mildest symptoms.

**AD-Related Regional Thinning Parallels the Topography of Neuropathology**

The spatial topography of cortical thinning in AD that we observed in vivo in the present study is consistent with the spatial distribution of neurodegenerative change known to occur in the disease from post-mortem studies (Brun and Gustafson 1976; Arnold et al. 1991; Braak and Braak 1991) and from recent in vivo PET investigations using tracers that bind to pathologic proteins (Klunk et al. 2004; Buckner et al. 2005; Mintun et al. 2006; Small et al. 2006). These regions also represent the major limbic and heteromodal cortical areas (Mesulam 1998).

The spatial topography of regional cortical thinning that we identified in mild AD is consistent with previous observations using voxel-based morphometry (Baron et al. 2001; Karas et al. 2003; Bozzali et al. 2006; Whitwell et al. 2008) and similar techniques (Thompson et al. 2001; Scahill et al. 2002; Buckner et al. 2005; Apostolova et al. 2007) as well as 2 previous investigations using cortical thickness techniques (Lev et al. 2005; Du et al. 2007). Generally, these efforts have converged upon a similar pattern of atrophy that is present in the medial temporal, lateral temporoparietal, and midline parietal regions, with variable findings in frontal regions. The major contribution of the present work relates to the demonstration of a consistent, stable estimate of the localization of relatively prominent cortical thinning in a large multicenter sample of mild AD patients, which can be used to predict the presence of thinning in milder and presymptomatic patient groups.

The magnitude of thinning within some regions is relatively large given the patients' mild level of dementia—even at early clinical stages of the illness, several regions are 10–20% thinner than normal. The regions with a larger degree of thinning—medial temporal, inferior temporal, temporal pole, inferior parietal, and posterior cingulate/precuneus—are those typically thought to be affected earliest in the course of the disease on the basis of the burden of pathologic accumulation (Hyman et al. 1984; Van Hoesen et al. 1986; Arnold et al. 1991; Arriagada, Gwinn-Duston, et al. 1992; Arriagada, Gwinn-Duston, et al. 1992; Arriagada, Marzloff, et al. 1992), neuronal loss, and gliosis (Brun and Gustafson 1976). A number of previous studies of cortical atrophy in AD have focused on spatial localization but have not estimated the magnitude of effects (Baron et al. 2001; Frisoni et al. 2002; Scahill et al. 2002; Buckner et al. 2005). Estimates of the magnitude of cortical atrophy have demonstrated the largest effects in temporal and parietal cortex (Karas et al. 2004; Du et al. 2007), with 15–20% thinning in caudal lateral temporal and posterior parietal cortex (Thompson et al. 2001, 2003; Leveque et al. 2005; Apostolova et al. 2007) as well as medial temporal cortex (Leveque et al. 2005). The results of the present study are quite consistent with these previous studies, and contribute by showing that similar but milder effects are present in patients with clinically milder forms of AD.
MRI Measures of Regional Cortical Thinning in AD Correlate with Severity of Symptoms of the Disease

Previous studies have shown that AD-related thinning of particular cortical regions correlates with worse performance on cognitive testing in patients spanning a relatively broad spectrum of clinical impairment, including a sizable number of moderately demented patients (Lerch et al. 2005; Du et al. 2007). In the present study, we specifically focused on the relatively narrow clinical spectrum of incipient, very mild, and mild AD, and investigated the relationship of regional cortical thickness to CDR-SB. The CDR-SB is a finely graded measure that reflects the clinician’s impression of the relative severity of cognitive symptoms that affect memory, orientation, judgment, and problem-solving, and daily function at home and in the community. It is widely used in clinical research, including trials of putative therapeutic agents. The CDR-SB is strongly associated with cortical thickness in many of the regions identified in this study, suggesting that progressive worsening of cognitive impairment within the very mild to mild spectrum of AD is associated with progressive thinning of specific heteromodal regions of the cortex. Because the CDR-SB is a clinical measure of impairment primarily reflecting symptom severity in daily life, our results support the clinical validity of regional cortical thickness measures as an imaging biomarker of AD severity.

Although the data in this study are cross-sectional, inferences can be made regarding the sequence of involvement of the cortical regions in the course of AD. Based on the analysis comparing the 4 groups of participants from Sample 1a and 1b, some regions, particularly ventromedial temporal and inferior parietal cortex, exhibit thinning even in the mildest (incipient AD) group, suggesting very early involvement. Other regions, particularly superior parietal and frontal cortex, do not show appreciable thinning until symptoms are more prominent (very mild to mild AD dementia), suggesting that they become involved later in the course of the disease (Scahill et al. 2002; Buckner et al. 2005). Similarly, from the within-group correlational analyses, symptom severity (CDR-SB) within the very mild AD patient group correlates with medial temporal and inferior parietal thinning, whereas symptom severity within the mild AD patient group correlates with thinning in frontal regions, again suggesting temporoparietal involvement prior to frontal involvement. These inferences are consistent with those made from pathologic studies (Arriagada, Marzloff, et al. 1992;
Braak et al. 1998), but longitudinal MRI data will be required for confirmation.

**Detection of cortical thinning in asymptomatic amyloid-positive individuals**

The development of technology to image fibrillar amyloid deposits in living individuals (Klunk et al. 2004) has led to the confirmation of findings from post-mortem studies (Tomlinson et al. 1968; Price et al. 1991; Bennett et al. 2006) that amyloid pathology may be present in some cognitively intact older individuals (Buckner et al. 2005; Mintun et al. 2006). The topographic distribution of amyloid in the neocortex appears to overlap in many respects that of atrophy in AD (Buckner et al. 2005).

We demonstrate here that subtle thinning is present in some AD cortical signature ROIs in a group of asymptomatic OC individuals who are amyloid-positive (Fig. 6). An aggregate measure of the thickness of the AD cortical signature regions in these asymptomatic older individuals revealed subtle thinning in comparison to the large group (N = 115) of OC individuals from Sample no. 1 whose amyloid status is unknown. The ability to detect thinning in these cortical regions in asymptomatic amyloid-positive individuals suggests that the approach to regional cortical thickness measurement outlined here may be useful as a biomarker of early disease, and it will be of great interest to follow such individuals longitudinally with both imaging and clinical assessments. It will also be important to demonstrate whether this putative imaging biomarker has reasonable sensitivity and specificity at the individual subject level.

**Regional Cortical Thinning in Mild AD is Consistent across 4 Patient Samples**

The consistency of regional cortical thinning across the 4 samples of mild AD patients is remarkable, despite a variety of sample- and instrument-related factors that could have contributed to variability. Sample-related factors that could increase variability of cortical thinning in AD include severity of clinical impairment, which in this study is relatively similar across the samples based on CDR and mental status test scores (yet these clinical measures themselves are associated with a certain level of unreliability across sites). Because diagnoses have been made clinically, the probable inclusion of some individuals in each sample with other pathologies in addition to (or instead of) AD could also increase variability of cortical thickness measures. Moreover, variability in cortical thickness across normal participants as well as AD patients can be influenced by age and sex (Salat et al. 2004), which do differ in these samples and although controlled for statistically may still have exerted subtle influence. Finally, and potentially most importantly, MRI instrument-related factors may contribute to variability, including scanner model, head coil, pulse sequence, and field strength. Across the 4 samples, the scanners were all made by the same manufacturer and employed versions of the same sequence, but the scanner models, head coils, and software operating systems differed, and one sample was scanned at 3.0 Tesla, whereas the others were scanned at 1.5 Tesla. Yet the variability in cortical thickness measures across the samples was remarkably low, as illustrated by the medial temporal cortex, the thickness of which ranged between 2.9 and 3.0 mm in the control groups of all 4 samples (Fig. 3, upper left graph). Variability within a single sample appears even lower, as can be seen by examining the primary visual cortex measure in the Washington University sample across the 4 clinical groups, which is centered almost exactly on 1.5 mm (Fig. 4, lower right graph). There are some regions in which variability of thinning across samples is higher, particularly superior parietal and inferior temporal, the origins of which are unclear but may relate to differences in the clinical characteristics of the samples, or to heterogeneity of levels of pathology. Further studies of the contributors to variability in cortical thickness estimates will be useful to better understand the potential effects of factors that did not vary in this study, such as scanner manufacturer or sequence (Han et al. 2006; Dickerson et al. 2008).

The consistency of AD-related cortical thinning across the multiple subject samples strongly supports the notion that pooling of multisite MRI data is feasible for cortical thickness analysis (Mueller et al. 2005; Murphy et al. 2006). Further support for this point is presented in Figure 5, which illustrates the cortical map derived from a combined analysis of the 267 participants in all 4 mildly impaired (CDR 1) samples. Regions in which the thickness of the cerebral cortex of AD patients is at least 0.15 mm thinner than OC are graded in terms of degree of thinning. This map illustrates the spatial topography of the effects quantified in Tables 3 and 4, showing that medial temporal cortex has the greatest magnitude of thinning, followed by temporal pole, inferior temporal, and inferior parietal cortex. Because it encompasses a large number of participants drawn from multiple samples, we believe it is the best current estimate of the degree of regional cortical thinning in mild AD. The map in Figure 5 depicts a spatial distribution of thinning magnitude that is remarkably similar to the map in Figure 2, which shows the statistical significance of the general linear model comparing thickness in AD versus OC. Regions may differ between the 2 maps because of variance, with some regions with relatively prominent thinning showing lesser statistical effects because of greater variance (e.g., posterior cingulate). Comparison of these 2 maps again reinforces the point that pooled analysis of multiple samples of MRI data can be used to robustly detect disease-related effects.

**Value of High-Throughput Automated MRI Data Analysis**

The MRI data analysis procedure used here to quantify cortical thickness in the 380 scans in the present study is nearly fully automated, with manual operator involvement at a few key processing steps for checking and minor corrections to, for example, the skull stripping procedure. Thus, this high-throughput data analysis system will likely lend itself well to analyses of large data sets from clinical trials or studies such as the ADNI. The quantitative measures of the thickness of the AD cortical signature regions identified in this study can be derived for individual participants and compared with a control group to assist in diagnosis or to establish a baseline for longitudinal comparison.

An important aspect of the analytic approach used in this study is that the ROIs were localized based on an exploratory analysis of the “disease effect” of AD across the entire cortical mantle without the use of a priori constraints tied to particular anatomic features of the cortex. That is, the ROIs were not delimited based on gyral crowns, sulcal fundi, or other elements of cortical folding patterns often used to demarcate cortical ROIs. The generation of “disease localizer” ROIs from an initial exploratory analysis, followed by the use of such localizers to test hypotheses in separate participant samples, is
analogous to the use of "functional localizers" in functional neuroimaging studies. Just as functionally specific cortical regions may not obey the constraints of cortical folding patterns (Eickhoff et al. 2006), neurodegenerative diseases may selectively affect subregions within larger traditional anatomic regions (e.g., precuneus), or may traverse the gyral or sulcal boundaries of ROIs defined using such landmarks.

Although a strength of the present study is its focus on mild clinical stages of AD, important limitations include the lack of longitudinal data and that the clinical diagnosis of AD is not supported by other imaging markers or by autopsy. It will be important to perform retrospective analyses of MRI data from individuals who have been demonstrated by autopsy to have definite AD with a typical pattern of pathology. It will also be of great interest to perform multimodal in vivo studies combining MRI measures of cortical thickness with imaging markers of pathology (Buckner et al. 2005). It is possible that in vivo pathologic markers may indicate, with a high degree of specificity, which individuals harbor AD pathology, but that MRI-derived measures of cortical thinning may be sensitive predictors of the emergence of clinical symptoms, but this hypothesis will require focused investigation.

Possible Biological Contributors to Cortical Thinning in AD
Studies of post-mortem tissue have shown that thickness is reduced in regions of the cerebral cortex that are affected pathologically in AD (Gomez-Isla et al. 1996; Regeur 2000). Although a few investigations have demonstrated that MRI-derived hippocampal volume correlates with neurofibrillary tangle burden in AD patients (Gosche et al. 2002; Jack et al. 2002; Silbert et al. 2003; Csernansky et al. 2004), the histologic determinants of cortical thinning are unknown. Some regions with prominent thinning identified in the present study are primarily affected by neurofibrillary tangles early in the course of the disease and to a much lesser degree by plaques (e.g., medial temporal cortex), whereas others carry a heavy burden of both major pathologic markers of AD (e.g., temporal pole and rostral inferior temporal gyrus) (Brun and Gustafson 1976; Arnold et al. 1991; Braak and Braak 1991; Arriagada, Marzloff et al. 1992). It is notable that regions in which amyloid deposition tends to be prominent from PIB imaging data (prefrontal, gyrus rectus, precuneus, lateral temporal) are not areas in which prominent thinning is found. Although cortical thinning may be an indicator of the burden of neurofibrillary tangles, neuritic plaques, or other pathology, it is likely a more global indicator of the disruption of the healthy anatomic configuration of the cortical mantle. This may be a sign of the loss of neuronal, glial, or other important cellular components such as neuropil volume, which reflects synaptic numbers and extent of dendritic branching, both of which are markedly reduced early in the course of AD (Coleman and Flood 1987; DeKosky and Scheff 1990; Scheff et al. 1990; DeKosky et al. 1996; Coleman et al. 2004) and relate to degree of cognitive impairment (Terry et al. 1991). Higher-resolution MRI data (Schleicher et al. 2005) will probably be required to test hypotheses (Arnold et al. 1991) about laminar-specific patterns of abnormalities in AD and related disorders.

Supplementary Material
Supplementary material can be found at: http://www.cercor.oxfordjournals.org/

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References


